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(54) N-TERMINALLY CHEMICALLY MODIFIED PROTEIN COMPOSITIONS AND METHODS

N-TERMINAL CHEMISCH MODIFIZIERTE PROTEIN-ZUSAMMENSETZUNGEN UND METHODEN
COMPOSITIONS DE PROTEINES AYANT SUBI UNE MODIFICATION CHIMIQUE A L'EXTREMITÉ
N-TERMINALE ET PROCEDES

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Description

[0001] The present invention relates to novel N-terminally monopegylated G-CSF compositions.

5 **Background**

[0002] Proteins for therapeutic use are currently available in suitable forms in adequate quantities largely as a result of the advances in recombinant DNA technologies. The availability of recombinant proteins has engendered advances in protein formulation and chemical modification. One goal of such modification is protein protection. Chemical attachment may effectively block a proteolytic enzyme from physical contact with the protein backbone itself, and thus prevent degradation. Additional advantages include, under certain circumstances, increasing the stability and circulation time of the therapeutic protein and decreasing immunogenicity. A review article describing protein modification and fusion proteins is Francis, *Focus on Growth Factors* 3: 4-10 (May 1992) (published by Mediscript, Mountview Court, Friem Barnet Lane, London N20, OLD, UK).

[0003] Polyethylene glycol ("PEG") is one such chemical moiety which has been used in the preparation of therapeutic protein products (the verb "pegylate" meaning to attach at least one PEG molecule). For example Adagen, a pegylated formulation of adenosine deaminase is approved for treating severe combined immunodeficiency disease; pegylated superoxide dismutase has been in clinical trials for treating head injury; pegylated alpha interferon has been tested in phase I clinical trials for treating hepatitis; pegylated glucocerebrosidase and pegylated hemoglobin are reported to have been in preclinical testing. The attachment of polyethylene glycol has been shown to protect against proteolysis, Sada, et al., *J. Fermentation Bioengineering* 71: 137-139 (1991), and methods for attachment of certain polyethylene glycol moieties are available. See U.S. Patent No. 4,179,337, Davis et al., "Non-Immunogenic Polypeptides," issued December 18, 1979; and U.S. Patent No. 4,002,531, Royer, "Modifying enzymes with Polyethylene Glycol and Product Produced Thereby," issued January 11, 1977. For a review, see Abuchowski et al., in *Enzymes as Drugs*, J.S. Holcberg and J. Roberts, eds. pp. 367-383 (1981).

[0004] Other water soluble polymers have been used, such as copolymers of ethylene glycol/propylene glycol, carboxymethylcellulose, dextran, polyvinyl alcohol, polyvinyl pyrrolidone, poly-1,3-dioxolane, poly-1,3,6-trioxane, ethylene/maleic anhydride copolymer, polyaminoacids (either homopolymers or random copolymers).

[0005] For polyethylene glycol, a variety of means have been used to attach the polyethylene glycol molecules to the protein. Generally, polyethylene glycol molecules are connected to the protein via a reactive group found on the protein. Amino groups, such as those on lysine residues or at the N-terminus, are convenient for such attachment. For example, Royer (U.S. Pat. No. 4,002,531, above) states that reductive alkylation was used for attachment of polyethylene glycol molecules to an enzyme. EP 0 539 167, published April 28, 1993, Wright, "Peg Imidates and Protein Derivates Thereof" states that peptides and organic compounds with free amino group(s) are modified with an immediate derivative of PEG or related water-soluble organic polymers. U.S. Patent No. 4,904,584, Shaw, issued February 27, 1990, relates to the modification of the number of lysine residues in proteins for the attachment of polyethylene glycol molecules via reactive amine groups.

[0006] One specific therapeutic protein which has been chemically modified is granulocyte colony stimulating factor, "G-CSF." G-CSF induces the rapid proliferation and release of neutrophilic granulocytes to the blood stream, and thereby provides therapeutic effect in fighting infection.

[0007] European patent publication EP 0 401 384, published December 12, 1990, entitled, "Chemically Modified Granulocyte Colony Stimulating Factor," describes materials and methods for preparing G-CSF to which polyethylene glycol molecules are attached.

[0008] Modified G-CSF and analogs thereof are also reported in EP 0 473 268, published March 4, 1992, entitled "Continuous Release Pharmaceutical Compositions Comprising a Polypeptide Covalently Conjugated To A Water Soluble Polymer," stating the use of various G-CSF and derivatives covalently conjugated to a water soluble particle polymer, such as polyethylene glycol.

[0009] A modified polypeptide having human granulocyte colony stimulating factor activity is reported in EP 0 335 423 published October 4, 1989.

[0010] Another example is pegylated IL-6, EP 0 442 724, entitled, "Modified hIL-6," which discloses polyethylene glycol molecules added to IL-6.

[0011] EP 0 154 316, published September 11, 1985 reports reacting a lymphokine with an aldehyde of polyethylene glycol.

[0012] Many methods of attaching a polymer to a protein involve using a moiety to act as a linking group. Such moieties may, however, be antigenic. A tresyl chloride method involving no linking group is available, but this method may be difficult to use to produce therapeutic products as the use of tresyl chloride may produce toxic by-products. See Francis et al., in: *Stability of protein pharmaceuticals: in vivo pathways of degradation and strategies for protein stabilization* (Eds. Ahern, T. and Manning, M.C.) Plenum, New York, 1991) Also, Delgado et al., "Coupling of PEG to

Protein By Activation With Tresyl Chloride, Applications In Immunoaffinity Cell Preparation*, In: Fisher et al., eds., Separations Using Aqueous Phase Systems, Applications In Cell Biology and Biotechnology, Plenum Press, N.Y.N.Y., 1989 pp. 211-213.

[0013] Charnow et al., Bioconjugate Chem. 5: 133-140 (1994) report the modification of CD4 immunoadhesin with monomethoxypoly(ethylene glycol) aldehyde via reductive alkylation. The authors report that 50% of the CD4-Ig was MePEG-modified under conditions allowing the control over the extent of pegylation. *Id.* at page 137. The authors also report that the *in vitro* binding capability of the modified CD4-Ig (to the protein gp 120) decreased at a rate correlated to the extent of MePEGylation. *Ibid.* See also, Rose et al., Bioconjugate Chemistry 2: 154-159 (1991) which reports the selective attachment of the linker group carbonylhydrazide to the C-terminal carboxyl group of a protein substrate (insulin).

[0014] None of the methods in the general state of the art, or the art relating to particular proteins, allow for selective attachment of a water soluble polymer to the N-terminus of a protein such as G-CSF, however. Rather, the currently existing methods provide for non-selective attachment at any reactive group, whether located within the protein, such as a lysine side group, or at the N-terminus. This results in a heterogeneous population of pegylated proteins. For example, for pegylated G-CSF molecules, some molecules have a different number of polyethylene glycol moieties than others. As an illustration, protein molecules with five lysine residues reacted in the above methods may result in a heterogeneous mixture, some having six polyethylene glycol moieties, some five, some four, some three, some two, some one and some zero. And, among the molecules with several, the polyethylene glycol moieties may not be attached at the same location on different molecules.

[0015] This is disadvantageous when developing a pegylated protein product for therapeutic purposes. In such development, predictability of biological activity is crucial. For example, it has been shown that in the case of nonselective conjugation of superoxide dismutase with polyethylene glycol, several fractions of the modified enzyme were completely inactive (P. McGoff et al. Chem. Pharm. Bull. 36:3079-3091 (1988)). One cannot have such predictability if the therapeutic protein differs in composition from lot to lot. Some of the polyethylene glycol moieties may not be bound as stably in some locations as others, and this may result in such moieties becoming dissociated with the protein. Of course, if such moieties are randomly attached and therefore become randomly dissociated, the pharmacokinetics of the therapeutic protein cannot be precisely predictable. From a consumer's point of view, the circulation time may vary from lot to lot, and thus dosing may be inaccurate. From a producer's point of view, garnering regulatory approval for sale of the therapeutic protein may have added complexities. Additionally, none of the above methods provide for selective N-terminal pegylation without a linking moiety (between the protein and the polymer). If a linking moiety is used, there may be disadvantages due to possible antigenicity.

[0016] Thus, there exists a need for methods for preparing N-terminally monopegylated G-CSF and analogs thereof. The present invention addresses this need in a number of aspects.

Summary of the Invention

[0017] The present invention relates to a substantially homogenous preparation of N-terminally monopegylated G-CSF or analogs thereof, and methods therefore. Unexpectedly, this chemical modification at the N-terminus of G-CSF demonstrated advantages in stability which are not seen in other G-CSF species containing one chemical modification at another location on the molecule. Also unexpectedly, in the present process for making N-terminally monopegylated G-CSF, it was found that using reductive alkylation, one could provide conditions for selectively modifying the N-terminus, and this method is broadly applicable to other proteins (or analogs thereof), as well as G-CSF. Also surprisingly, using reductive alkylation, the end product -- G-CSF with an amine linkage to the water soluble polymer -- was found to be far more stable than an identical polymer/protein conjugate having an amide linkage.

[0018] In one aspect, the present invention relates to a substantially homogenous preparation of N-terminally monopegylated G-CSF or an analog thereof. One working example below demonstrates that N-terminally monopegylated G-CSF is more stable than other types of monopegylated G-CSF. Additionally, since the N-terminus of the G-CSF molecule is more available during reaction with polyethylene glycol, a higher proportion of the N-termini are pegylated, and therefore, this species provides processing advantages.

[0019] The present invention also relates to a type of reductive alkylation which selectively activated the α -amino group of the N-terminus of G-CSF or an analog thereof, thereby providing for selective attachment of a water soluble PEG moiety at the N-terminus. This provides for a substantially homogenous preparation of polymer/protein conjugate molecules as well as a preparation of pegylated G-CSF molecules having the polyethylene glycol moiety directly coupled to the protein moiety. This method is described below for G-CSF, and this provides for additional aspects of the present invention.

Brief Description of the Drawings

[0020] FIGURE 1A is a reproduction of the chromatogram of the peaks from ion exchange chromatography of pegylated G-CSF.

[0021] FIGURE 1B is an SDS-PAGE of various species of monopegylated G-CSF.

[0022] FIGURE 2 is an SEC-HPLC profile of (Line A) recombinant human methionyl G-CSF standard; (Line B) SCM-PEG-G-CSF reaction mix; (Line C) N-terminally pegylated G-CSF; (Line D) lysine 35 monopegylated G-CSF; (Line E) lysine 41 monopegylated G-CSF.

[0023] FIGURES 3A, 3B, and 3C are HPLC endoproteinase SV8 peptide mapping tracings of (3A) N-terminally pegylated G-CSF; (3B) lysine 35 monopegylated G-CSF; (3C) lysine 41 monopegylated G-CSF.

[0024] FIGURE 4 is a bar graph illustrating a comparison of *in vitro* bioactivity of monopegylated G-CSF species compared to an unpegylated standard.

[0025] FIGURES 5A and 5B are graphs illustrating results of *in vivo* bioactivity assays of monopegylated G-CSF derivatives, with (5A) illustrating the average hamster white blood cell count after a single subcutaneous injection of N-terminally pegylated G-CSF, lysine 35 monopegylated G-CSF, or lysine 41 monopegylated G-CSF, and (5B) illustrating the net average white blood cell count area under the curve after a single subcutaneous injection of the various monopegylated G-CSF derivatives listed above.

[0026] FIGURES 6A, 6B, and 6C are SEC-HPLC profiles for stability studies of N-terminally pegylated G-CSF or lysine 35 monopegylated G-CSF. FIGURES 6A and 6B are the profiles for stability studies conducted at pH 6.0 at 4°C for (6A) N-terminally monopegylated G-CSF or (6B) lysine 35 monopegylated G-CSF. FIGURE 6C shows the profiles for extended stability studies at pH 6.0 and 4°C for lysine 35 monopegylated G-CSF, Time ("T"), indicates days.

[0027] FIGURE 7 illustrates size exclusion HPLC analysis of the reaction mixture in the process of reductive alkylation of rh-G-CSF with methoxypolyethylene glycol aldehyde (MW 6 kDa).

[0028] FIGURE 8 illustrates size exclusion HPLC analysis of the reaction mixture using N-hydroxysuccinimidyl ester of MPEG, also at MW=6kDa.

[0029] FIGURE 9 illustrates the total white blood cell response after a single subcutaneous dose to mono-N terminal MPEG-G-CSF conjugates prepared by reductive alkylation of rh-G-CSF with MPEG aldehydes of different molecular weights (6 kDa, 12 kDa and 20 kDa).

Detailed Description

[0030] In one aspect, the present invention relates to N-terminally monopegylated G-CSF compositions and methods therefor.

[0031] The present methods (for both N-terminally modified G-CSF as well as the present reductive alkylation method) provide for a substantially homogenous mixture of monopolymer/protein conjugate. "Substantially homogenous" as used herein means that the only polymer/protein conjugate molecules observed are those having one polymer moiety. The preparation may contain unreacted (i.e., lacking polymer-moiety) protein. As ascertained by peptide mapping and N-terminal sequencing, one example below provides for a preparation which is at least 90% monopolymer/protein conjugate, and at most 10% unreacted protein. Preferably, the N-terminally monopegylated material is at least 95% of the preparation (as in the working example below) and most preferably, the N-terminally monopegylated material is 99% of the preparation or more. The monopolymer/protein conjugate has biological activity. The present "substantially homogenous" N-terminally pegylated G-CSF preparations provided herein are those which are homogenous enough to display the advantages of a homogenous preparation, e.g., ease in clinical application in predictability of lot to lot pharmacokinetics.

[0032] One may choose to prepare a mixture of polymer/protein conjugate molecules, and the advantage provided herein is that one may select the proportion of monopolymer/protein conjugate to include in the mixture. Thus, if desired, one may prepare a mixture of various proteins with various numbers of polymer moieties attached (i.e., di-, tri-, tetra-, etc.) and combine this mixture with the monopolymer/protein conjugate material prepared using the present methods, and have a mixture with a predetermined proportion of monopolymer/protein conjugate.

[0033] Provided below is a working example using G-CSF, which, as described above, is a therapeutic protein used to treat hematopoietic disorders. In general, G-CSF useful in the practice of this invention may be a form isolated from mammalian organisms or, alternatively, a product of chemical synthetic procedures or of prokaryotic or eukaryotic host expression of exogenous DNA sequences obtained by genomic or cDNA cloning or by DNA synthesis. Suitable prokaryotic hosts include various bacteria (e.g., *E. coli*); suitable eukaryotic hosts include yeast (e.g., *S. cerevisiae*) and mammalian cells (e.g., Chinese hamster ovary cells, monkey cells). Depending upon the host employed, the G-CSF expression product may be glycosylated with mammalian or other eukaryotic carbohydrates, or it may be non-glycosylated. The G-CSF expression product may also include an initial methionine amino acid residue (at position -1). The present invention contemplates the use of any and all such forms of G-CSF, although recombinant G-CSF, especially

E. coli derived, is preferred, for, among other things, greatest commercial practicality.

[0034] Certain G-CSF analogs have been reported to be biologically functional, and these may also be N-terminally monopegylated in accordance with the present invention. G-CSF analogs are reported in U.S. Patent No. 4,810,643. Examples of other G-CSF analogs which have been reported to have biological activity are those set forth in AU-A-76380/91, EP 0 459 630, EP 0 272 703, EP 0 473 268 and EP 0 335 423, although no representation is made with regard to the activity of each analog reportedly disclosed. See also AU-A-10948/92, PCT US94/00913 and EP 0 243 153.

[0035] Generally, the G-CSFs and analogs thereof useful in the present invention may be ascertained by practicing the chemical modification procedures as provided herein to selectively chemically modify the N-terminal α -amino group, and testing the resultant product for the desired biological characteristic, such as the biological activity assays provided herein. Of course, if one so desires when treating non-human mammals, one may use recombinant non-human G-CSF's, such as recombinant murine, bovine, canine, etc. See PCT WO 91/05798 and PCT WO 89/10932, for example.

[0036] Thus, another aspect of the present invention includes N-terminally monopegylated G-CSF analog compositions. As described above, G-CSF analogs may include those having amino acid additions, deletions and/or substitutions (as compared to the G-CSF amino acid sequence set forth in Example 1, below). Those G-CSF analogs which are predicted to function when N-terminally pegylated to selectively stimulate the production of neutrophils are those with an N-terminus which is not necessary for binding to a G-CSF receptor. See Hill et al., PNAS-USA 90: 5167-5171 (1993); see also PCT US94/00913.

[0037] The polyethylene glycols used may be selected from among water soluble polymers. So that the protein to which it is attached does not precipitate in an aqueous medium, such as a physiological medium. For reductive alkylation, the polymer selected should have a single reactive aldehyde group so that the degree of polymerization may be controlled as provided for in the present methods. The polymer may be branched or unbranched. Preferably, for therapeutic use of the end-product preparation, the polymer will be pharmaceutically acceptable. One skilled in the art will be able to select the desired polymer based on such considerations as whether the polymer/protein conjugate will be used therapeutically, and if so, the desired dosage, circulation time, resistance to proteolysis, and other considerations. For G-CSF, these may be ascertained using the assays provided herein, and one skilled in the art should select the appropriate assays for other therapeutic proteins.

[0038] Subject to considerations for optimization as discussed below, the polymer may be of any molecular weight, and may be branched or unbranched. For polyethylene glycol, the preferred molecular weight is between about 2kDa and about 100kDa, preferably between about 2 and 25 KDa (the term "about" indicating that in preparations of polyethylene glycol, some molecules will weigh more, some less, than the stated molecular weight). Examples 1 and 2 below involve the use of PEG 6000, which was selected for ease in purification and for providing an adequate model system. PEG of other molecular weights may be used, depending on the desired therapeutic profile (e.g., the duration of sustained release desired, the effects, if any on biological activity, the ease in handling, the degree or lack of antigenicity and other known effects of the polyethylene glycol to a therapeutic protein or analog).

[0039] One specific aspect of the present invention is N-terminally monopegylated G-CSF comprised of a polyethylene glycol moiety and a G-CSF moiety. For the present compositions, one may select from a variety of polyethylene glycol molecules (by molecular weight, branching, etc.), the proportion of polyethylene glycol molecules to G-CSF protein molecules in the reaction mix, the type of pegylation reaction to be performed, the method of obtaining the selected N-terminally pegylated G-CSF, and the type of G-CSF to be used. Further, the present compositions and methods include formulation of pharmaceutical compositions, methods of treatment and manufacture of medicaments.

[0040] The proportion of polyethylene glycol molecules to protein molecules will vary, as will their concentrations in the reaction mixture. In general, the optimum ratio (in terms of efficiency of reaction in that there is no excess unreacted protein or polymer) will be determined by the molecular weight of the polyethylene glycol selected. In addition, as one example of the present methods involves non-specific pegylation and later purification of N-terminally monopegylated species, the ratio may depend on the number of available reactive groups (typically alpha or epsilon amino groups) available. One working example herein involved a fairly low reaction ratio of protein:PEG molecules to obtain mono-pegylated material generally (1.5 PEG molecules per protein molecules).

[0041] For obtaining N-terminally monopegylated G-CSF, the method for pegylation may also be selected from among various methods, as discussed above, or the present reductive alkylation as described in Example 2, below. A method involving no linking group between the polyethylene glycol moiety and the protein moiety is described in Francis et al., In: Stability of protein pharmaceuticals: in vivo pathways of degradation and strategies for protein stabilization (Eds. Ahern, T. and Manning, M.C.) Plenum, New York, 1991) Also, Delgado et al., "Coupling of PEG to Protein By Activation With Tresyl Chloride, Applications In Immunoaffinity Cell Preparation", In: Fisher et al., eds., Separations Using Aqueous Phase Systems, Applications In Cell Biology and Biotechnology, Plenum Press, N.Y.N.Y., 1989 pp. 211-213, involves the use of tresyl chloride, which results in no linkage group between the polyethylene glycol moiety and the protein moiety. This method may be difficult to use to produce therapeutic products as the use of tresyl chloride may produce toxic by-products. One of the present working examples involves the use of N-hydroxy succinimidyl (NHS)

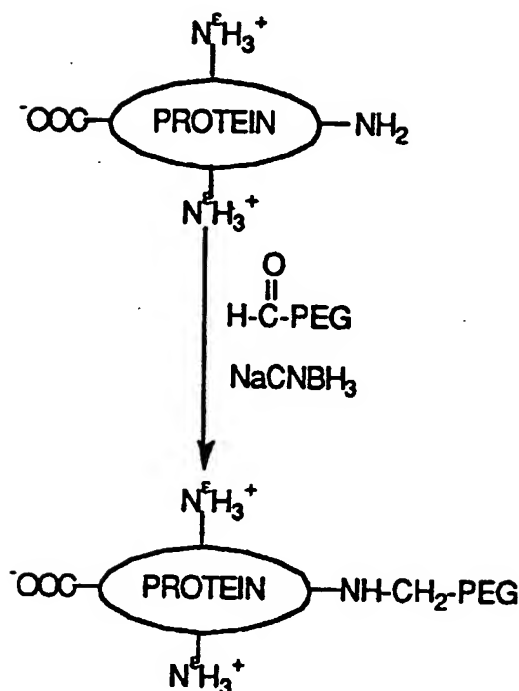
esters of carboxymethyl methoxy polyethylene glycol. As will be discussed in more detail below, another working example involves the use of the present reductive alkylation methods.

[0042] The method of obtaining the N-terminally monopegylated G-CSF preparation (i.e., separating this molecule from other monopegylated molecules if necessary) may be by purification of the N-terminally pegylated material from a population of pegylated G-CSF molecules. For example, presented below is an example where pegylated G-CSF is first separated by ion exchange chromatography to obtain material having a charge characteristic of monopegylated material (other multi-pegylated material having the same apparent charge may be present), and then the mono-pegylated materials are separated using size exclusion chromatography. In this way, N-terminally monopegylated G-CSF was separated from other monopegylated species, as well as other multi-pegylated species. Other methods are reported. For example, PCT WO 90/04606, published May 3, 1990, reports a process for fractionating a mixture of PEG-protein adducts comprising partitioning the PEG/protein adducts in a PEG-containing aqueous biphasic system.

[0043] In a different aspect, the present invention provides a method for selectively obtaining an N-terminally mono-pegylated G-CSF or an analog thereof. Provided below is a method of protein modification by reductive alkylation which exploits differential reactivity of different types of primary amino groups (lysine versus the N-terminal) available for derivatization in a particular protein. Under the appropriate reaction conditions, substantially selective derivatization of the protein at the N-terminus with a carbonyl group containing polymer is achieved. The reaction is performed at pH which allows one to take advantage of the pK_a differences between the epsilon-amino groups of the lysine residues and that of the alpha-amino group of the N-terminal residue of the protein. By such selective derivatization attachment of a water soluble PEG to the protein is controlled: the conjugation with the polymer takes place predominantly at the N-terminus of the protein and no significant modification of other reactive groups, such as the lysine side chain amino groups, occurs.

[0044] Importantly, and surprisingly, the present invention provides for a method of making a substantially homogeneous preparation of monopolymer/protein conjugate molecules, in the absence of further extensive purification as is required using other chemical modification chemistries. Additionally, the product having an amine linkage is unexpectedly more stable than a product produced with an amide linkage, and this is demonstrated in the aggregation studies below. More specifically, if polyethylene glycol is used, the present invention also provides for N-terminally mono-pegylated G-CSF or its analogs lacking possibly antigenic linkage groups, and having the polyethylene glycol moiety directly coupled to the protein moiety without toxic by-products.

[0045] The reaction may be diagrammed as follows indicating sodium cyanohydroboride as an illustrative reducing agent:



[0046] Thus, one aspect of the present invention is a method for preparing a polymer G-CSF conjugate comprised of (a) reacting the protein having more than one amino group with a water soluble polymer under reducing alkylation conditions, at a pH suitable to selectively activate the α -amino group at the amino terminus of said protein moiety so that said water soluble polymer selectively attaches to said α -amino group; and (b) obtaining the reaction product. One may optionally, and preferably for a therapeutic product, separate the reaction products from unreacted molecules.

[0047] For a substantially homogenous population of monopolymer/G-CSF conjugate molecules, the reaction conditions are those which permit the selective attachment of the water soluble polymer to the N-terminus of the G-CSF. Such reaction conditions generally provide for pK_a differences between the lysine amino groups and the α -amino group at the N-terminus (the pK being the pH at which 50% of the amino groups are protonated and 50% are not).

[0048] The pH also affects the ratio of PEG to G-CSF to be used. In general, if the pH is lower than the pK , a larger excess of polymer to protein will be desired (i.e., the less reactive the N-terminal α -amino group, the more polymer molecules are needed to achieve optimal conditions). If the pH is higher than the pK , the polymer:protein ratio need not be as large (i.e., more reactive groups are available, so fewer polymer molecules are needed).

[0049] Another important consideration is the molecular weight of the polymer. In general, the higher the molecular weight of the polymer, the fewer number of polymer molecules which may be attached to the protein. Similarly, branching of the polymer should be taken into account when optimizing these parameters. Generally, the higher the molecular weight (or the more branches) the higher the polymer:protein ratio.

[0050] For the present reductive alkylation, the reducing agent should be stable in aqueous solution and preferably be able to reduce only the Schiff base formed in the initial process of reductive alkylation. Preferred reducing agents may be selected from the group consisting of sodium borohydride and sodium cyanoborohydride. Sodium cyanoborohydride was used in the working examples below.

[0051] The water soluble PEG polymer may be of the type described above, and should have a single reactive aldehyde for coupling to the protein. For polyethylene glycol, use of PEG 6000 for coupling to G-CSF is described below. It is noted, that for G-CSF, PEG 12000, 20000 and 25000 have also been used successfully in the present methods. Polyethylene glycol propionaldehyde (see, e.g., U.S. Patent No. 5,252,714) is advantageous for its stability in water.

[0052] Thus, for the present N-terminally chemically modified G-CSF, any of the G-CSF's or analogs as described herein may be used (e.g., those described *supra*). The working examples below use recombinant G-CSF produced in bacteria, having 174 amino acids and an extra N-terminal methionyl residue.

[0053] In yet another aspect of the present invention, provided are pharmaceutical compositions of the above. Such pharmaceutical compositions may be for administration for injection, or for oral, pulmonary, nasal or other forms of administration. In general, comprehended by the invention are pharmaceutical compositions comprising effective amounts of monopolymer/protein conjugate products of the invention together with pharmaceutically acceptable diluents, preservatives, solubilizers, emulsifiers, adjuvants and/or carriers. Such compositions include diluents of various buffer content (e.g., Tris-HCl, acetate, phosphate), pH and ionic strength; additives such as detergents and solubilizing agents (e.g., Tween 80, Polysorbate 80), anti-oxidants (e.g., ascorbic acid, sodium metabisulfite), preservatives (e.g., Thimersol, benzyl alcohol) and bulking substances (e.g., lactose, mannitol); incorporation of the material into particulate preparations of polymeric compounds such as polylactic acid, polyglycolic acid, etc. or into liposomes. Such compositions may influence the physical state, stability, rate of *in vivo* release, and rate of *in vivo* clearance of the present N-terminally chemically modified proteins. See, e.g., Remington's Pharmaceutical Sciences, 18th Ed. (1990, Mack Publishing Co., Easton, PA 18042) pages 1435-1712.

[0054] In yet another aspect of the present invention, methods of manufacture of a medicament are provided. Conditions alleviated or modulated by the administration of the present polymer/G-CSF conjugates or analogs having the hematopoietic biological properties of naturally occurring G-CSF are typically those characterized by a reduced hematopoietic or immune function, and, more specifically, a reduced neutrophil count. Such conditions may be induced as a course of therapy for other purposes, such as chemotherapy or radiation therapy. Such conditions may result from infectious disease, such as bacterial, viral, fungal or other infectious disease. For example, sepsis results from bacterial infection. Or, such condition may be hereditary or environmentally caused, such as severe chronic neutropenia or leukemias. Age may also play a factor, as in the geriatric setting, patients may have a reduced neutrophil count or reduced neutrophil mobilization. Some of such conditions are reviewed in Filgrastim (r-met Hu G-CSF) in Clinical Practice, Morstyn, G. and T.M. Dexter, eds., Marcel Dekker, Inc., N.Y., N.Y. (1993), 351 pp. Other less-studied conditions which may be alleviated or modulated by administration of the present polymer/G-CSF conjugates may include the reduction of lipids or cholesterol in the blood stream, and certain cardiovascular conditions, as G-CSF may induce production of plasminogen activators. The mode of action of G-CSF or analogs thereof in these settings is not well understood at present. The addition of a water soluble polymer, such as polyethylene glycol, may provide practical patient benefits in that the sustained duration of biological activity may allow for fewer G-CSF injections per course of treatment.

[0055] For all of the above molecules, as further studies are conducted, information will emerge regarding appropriate dosage levels for treatment of various conditions in various patients, and the ordinary skilled worker, considering the therapeutic context, age and general health of the recipient, will be able to ascertain proper dosing. Generally, for injection or infusion, dosage will be between 0.01 µg/kg body weight, (calculating the mass of the protein alone, without chemical modification), and 100 µg/kg (based on the same).

[0056] The examples illustrate the various aspects discussed above. In Example 1, the advantages of N-terminally monopegylated G-CSF are demonstrated as compared to G-CSF monopegylated at lysine 35 or lysine 41 (of the G-CSF met + 174 amino acid version). Example 2 illustrates the present reductive alkylation in the preparation of N-terminally monopegylating G-CSF. The method provides for a substantially homogenous preparation of N-terminally monopegylated G-CSF.

EXAMPLE 1

A. Preparation of Recombinant Human met-G-CSF

[0057] Recombinant human met-G-CSF (referred to as "rhG-CSF" or "r-met-hu-G-CSF" from time to time herein) was prepared as described above according to methods in the Souza patent, U.S. Pat. No., 4,810,643. The rhG-CSF employed was an *E. coli* derived recombinant expression product having the amino acid sequence encoded by the DNA sequence shown below (Seq.ID NOs. 1 and 2):

5 ATG ACT CCA TTA GGT CCT GCT TCT TCT CTG CCG CAA AGC TTT CTG
 M T P L G P A S S L P Q S F L
 CTG AAA TGT CTG GAA CAG GTT CGT AAA ATC CAG GGT GAC GGT GCT
 L K C L E Q V R K I Q G D G A
 GCA CTG CAA GAA AAA CTG TGC GCT ACT TAC AAA CTG TGC CAT CCG
 A L Q E K L C A T Y K L C H P
 10 GAA GAG CTG GTA CTG CTG GGT CAT TCT CTT GGG ATC CCG TGG GCT
 E E L V L L G H S L G I P W A
 CCG CTG TCT TCT TGT CCA TCT CAA GCT CTT CAG CTG GCT GGT TGT
 P L S S C P S Q A L Q L A G C
 15 CTG TCT CAA CTG CAT TCT GGT CTG TTC CTG TAT CAG GGT CTT CTG
 L S Q L H S G L F L Y Q G L L
 CAA GCT CTG GAA GGT ATC TCT CCG GAA CTG GGT CCG ACT CTG GAC
 Q A L E G I S P E L G P T L D
 20 ACT CTG CAG CTA GAT GTA GCT GAC TTT GCT ACT ACT ATT TGG CAA
 T L Q L D V A D F A T T I W Q
 25 CAG ATG GAA GAG CTC GGT ATG GCA CCA GCT CTG CAA CCG ACT CAA
 Q M E E L G M A P A L Q P T Q
 GGT GCT ATG CCG GCA TTC GCT TCT GCA TTC CAG CGT CGT GCA GGA
 G A M P A F A S A F Q R R A G
 30 GGT GTA CTG GTT GCT TCT CAT CTG CAA TCT TTC CTG GAA GTA TCT
 G V L V A S H L Q S F L E V S
 TAC CGT GTT CTG CGT CAT CTG GCT CAG CCG TAA TAG
 Y R V L R H L A Q P * *

This was also the non-pegylated composition used for the control animals. Alternatively one may use purchased Neupogen® for the following pegylation procedures.

B. Preparation of Pegylated G-CSF

[0058] A 10 mg/ml solution of the above rhG-CSF, in 100 mM Bicine pH 8.0, was added to solid SCM-MPEG (N-hydroxy succinimidyl esters of carboxymethyl methoxy polyethylene glycol) (Union Carbide) with an average molecular weight of 6000 Daltons. This gave a 1.5 molar excess of SCM-MPEG to rhG-CSF. After one hour with gentle stirring, the mixture was diluted to 2 mg/ml with sterile water, and the pH was adjusted to 4.0 with dilute HCl. The reaction was carried out at room temperature. At this stage, the reaction mixture consisted mainly of three forms of monopegylated rhG-CSF, some dipegylated rhG-CSF, unmodified rhG-CSF and reaction bi-product (N-hydroxy succinimide).

C. Preparation of N-terminally Pegylated rhG-CSF

[0059] The three forms of monopegylated rhG-CSF were separated from each other using ion exchange chromatography. The reaction mixture was loaded (1 mg protein/ml resin) onto a Pharmacia S Sepharose FF column (Pharmacia XK50/30 reservoir, bed volume of 440 ml) equilibrated in buffer A (20 mM sodium acetate, pH 4.0). The column was washed with 3 column volumes of buffer A. The protein was eluted using a linear gradient from 0-23% buffer B (20 mM sodium acetate, pH 4.0, 1 M NaCl) in 15 column volumes. The column was then washed with one column volume of 100% buffer B and reequilibrated with 3 column volumes of buffer A. The flow rate for the entire run was maintained at 8 ml/min. The eluent was monitored at 280 nm and 5 ml fractions were collected. Fractions containing the individual monopegylated species were pooled according to FIGURE 1A. These pools were concentrated with a 350 mL Amicon stirred cell using a YM10 76 mm membrane.

[0060] Pooled fractions from the ion exchange chromatography were subjected to size exclusion chromatography to separate dipegylated species from monopegylated species. Typically, 5-10 mg in 2-5 ml of solution were loaded onto a 120 ml Pharmacia Superdex 75 HR 16/60 column equilibrated with 20 mM sodium acetate pH 4.0. The column was run at 1.5 ml/min for 100 min. Two ml fractions were collected. The protein content of the eluent was monitored at 280 nm. Fractions from separated peaks were pooled and subjected to analysis. The table below compares the proportional yields for each peak.

TABLE 1

Relative Yields and Site of Modification		
Site of Modification	Figure 1A Reference	Relative Yields
N-Terminus	Peak 1A	3
Lysine-35	Peak 2A	2
Lysine-41	Peak 3A	1

[0061] Under these conditions, the lysines at positions 17 and 24 probably were not significantly pegylated.

D. Characterization

[0062] Five analyses were done to characterize each sample: (1) SDS-Page (Figure 1B), (2) Size exclusion chromatography HPLC ("SEC-HPLC") (Figure 2), (3) peptide mapping analysis (Figures 3A, 3B, and 3C), (4) *in vitro* G-CSF bioassay (Figure 4), and (5) *in vivo* testing in hamster (Figures 5A and 5B).

[0063] With regard to the composition of each sample, results demonstrate that, of the N-terminally monopegylated G-CSF, the samples showed a greater than 95% N-terminally pegylated composition, with the remainder probably being unpegylated material (although the remainder of the samples is lower than the detection limit of the assay). With regard to the percent monopegylated for each of the three types of monopegylated material (N-terminal, pegylated at lysine 35, and pegylated at lysine 41), the N-terminal and the lysine 41 demonstrated greater than 97% monopegylated, and the lysine 35 pegylated material being somewhat lower, probably due to the instability of the molecule in the assay conditions. To summarize, the following results were obtained:

TABLE 2

Percent Composition of N-terminally pegylated G-CSF			
	Non-Reduced SDS PAGE	SEC-HPLC	N-Terminal Sequencing*
Monopegylated G-CSF	97.44	99.43	96.6
Unmodified G-CSF	2.56	0.57	3.4

* The N-terminal sequencing, as discussed *infra* is not here considered quantitative, as there may have been cleavage of the polyethylene glycol molecule from the N-terminus of the protein during the sequencing process.

TABLE 3

Percent Monopegylated for Three Species			
	N-terminal PEG-G-CSF (RI/UV=.96)*	LYS35 PEG-G-CSF** (RI/UV=.72)	LYS41 PEG-G-CSF (RI/UV=1.12)
Non-reduced SDS-PAGE	97.44	77.41	100.00
SEC HPLC	99.43	93.38	99.96

* RI/UV refers to the Index of Refraction/Ultraviolet light absorbance ratio, and is used to estimate the number of polyethylene glycol molecules per molecule of protein. It is calculated from the SEC-HPLC data using an Index of Refraction for polyethylene glycol and an ultraviolet absorbance for protein.

** Note that this species is unstable under the assay conditions used.

METHODS

[0064]

1. SDS-PAGE. SDS-PAGE was carried out in a non-reduced 4-20% ISS Daiichi Pure Chemicals, Co., Tokyo, Japan minigel using a Coomassie Brilliant Blue R-250 stain. The gel was scanned using a molecular Dynamics Densitometer with Image Quant. Results: Results are presented in FIGURE 1B. Lane number 1 (from the left hand side) included molecular weight protein standards (Novex Mark 12 Molecular Weight Standards). Lane 2 contains 3 µg rh-G-CSF standard. Lane 3 contains the SCM-PEG-G-CSF reaction mix, with 10 µg loaded. Lane 4 contains N-terminally monopegylated G-CSF, with 10 µg loaded. Lane 5 contains 10 µg of monopegylated G-CSF with the pegylation site at the lysine found at the 35th residue from the N-terminal methionine. Lane 6 contains 10 µg of monopegylated G-CSF with the pegylation site at the lysine found at the 41st residue from the N-terminal methionine. As can be seen, Lane 3, containing the N-terminally monopegylated material, shows a single band.

2. Size Exclusion Chromatography-High Pressure Liquid Chromatography. SEC-HPLC was carried out using a Waters HPLC system with a Biosep SEC 3000 column, using 100 mM sodium phosphate, pH 6.9, 1 ml/min for 20 minutes. The signal was monitored at 280 nm. Results: As can be seen from Figure 2, line "C," containing the N-terminally monopegylated rh-G-CSF contains a single peak, as do lines "D" (Lys-35 monopegylated material) and "E" (Lys-41 monopegylated material). This indicates substantial purity among the separated fractions of monopegylated G-CSF.

3. Peptide mapping. The following methods were used. Three samples, called "Mono-PEG-1" "Mono-PEG-2", and "Mono-PEG-3", were analyzed. (a) Reductive alkylation. 500 µg aliquots of mono-PEG-G-CSF were speed vac dried and reconstituted to a concentration of 1 mg in 950 µl in 0.3 M Tris-HCl containing 6 M Guanidinium HCl and 1 mM EDTA, pH 8.4. Samples were then 5-carboxymethylated by adding iodoacetic acid and incubated at 37°C for 20 minutes. Samples were then desalted using Sephadex G-25 Quick Spin Protein Columns and buffer exchanged. After desalting and buffer exchange, sample concentration was adjusted to 0.5 mg/ml using additional buffer. (b) Endoproteinase SV8 digestion. Samples were digested with SV8 (enzyme to substrate ratio of 1:25) at 25°C for 26 hours. (c) HPLC peptide mapping. Protein digests were injected onto a Vydac C4 column (4.6 x 250 mm, 5 µ particle size, 300 Å pore size) and peptides were mapped by HPLC using a linear gradient of acetonitrile in 0.1% TFA. Peptides were manually collected and dried in a Speed Vac for sequence analysis. Results: As compared to a reference standard, (i) (FIGURE 3A) for "Mono-PEG-1", (the N-terminally monopegylated material), a peak at 57.3 minutes diminished and a new peak appeared at 77.5 minutes; (ii) (FIGURE 3B) for "Mono-PEG-2", (the lysine 35 pegylated material), there was a decrease in peak height for a peptide with a retention time of 30.3 minutes, and a new peak eluted at 66.3 minutes; (iii) (FIGURE 3C) for "Mono-PEG-3" (the lysine 41 pegylated material), the peak at retention time of 30.3 minutes was missing, and a new peak appeared at 66.4 minutes. These peptides were the only significant differences in the sample maps. There were some small incomplete cleavages seen on either side of the peptide at 86.1 minutes due to minor digestion differences.

(d) N-terminal sequence analysis. Each of the "new" peptides in the above maps were N-terminally sequenced for identification. The dried peptides were reconstituted in 0.1% TFA and sequenced on an ABI protein sequencer. For "Mono-PEG-1" (the N-terminally monopegylated material), 60% of the "new" peak (at 77.5 minutes) was sequenced for 10 cycles. The initial yield was less than 5%, indicating that the N-terminal methionyl residue is blocked by a polyethylene glycol molecule. It is noted that this initial peptide should have resulted in a zero initial yield, and the <5% yield observed may be from detachment of the polyethylene glycol from the N-terminal methionyl group during sequence analysis. The sequence detected was that of the N-terminal peptide, M-T-P-L-G-P-A-S-S. For "Mono-PEG-2", (the lysine 35 pegylated material), 80% of the total peak volume was collected for the peak at 66.3 minutes, and was sequenced for 9 cycles. The recovery of lysine 35 was significantly low, indicating pegylation at position 35. The recovery of lysine 41 was consistent with the other residue, indicating no modification of this position. The peptide at 30.3 minutes decreased in peak height compared to the corresponding peak in the standard reference map. The peptide at 30.3 minutes is only 57.5% of the peak area of the corresponding peptide. The sequence detected for this species was K-L-C-A-T-Y-K-L. For "Mono-PEG-3", the lysine 41 material, 80% of the total peak volume collected for the peptide eluting at 66.4 minutes was sequenced for 9 cycles. The sequence detected was K-L-C-A-T-Y-K-L, and contained lysine residues 35 and 41. The recovery of lysine 35 was consistent with other residue recoveries. The recovery of lysine 41 was significantly lower indicating pegylation at position 41. Results: "Mono-PEG-1" is a N-terminally monopegylated material; "Mono-PEG-2" is a lysine 35 partially pegylated material; and "Mono-PEG-3" is a lysine 41 pegylated material. By comparing both the reference standard (non-pegylated G-CSF) and G-CSF monopegylated 1, 2, and 3 peptide maps, it was found that both the "Mono-PEG-2" (lysine 35) and "Mono-PEG-3" (lysine 41) maps exhibit slightly diminished peak heights for the N-terminal peptide. This indicates that the lysine 35 and lysine 41 pegylated material contains a small amount of N-terminally pegylated material or that the N-terminal methionine group has a small percentage of pegylation.

4. In vitro activity. The material was active. FIGURE 4 illustrates the results of in vitro assays. As can be seen, the N-terminally monopegylated material had 68% of the activity of non-modified rhG-CSF.

Methods: The G-CSF in vitro bioassay is a mitogenic assay utilizing a G-CSF dependent clone of murine 32D cells. Cells were maintained in Iscoves medium containing 5% FBS and 20 ng/ml rhG-CSF. Prior to sample addition, cells were prepared by rinsing twice with growth medium lacking rhG-CSF. An extended twelve point rhG-CSF standard curve was prepared, ranging from 48 to 0.5ng/ml (equivalent to 4800 to 50 IU/ml). Four dilutions, estimated to fall within the linear portion of the standard curve, (1000 to 3000 IU/ml), were prepared for each sample and run in triplicate. Because of their apparent lower activity in vitro, the pegylated rhG-CSF samples were luted approximately 4-10 times less. A volume of 40 μ l of each dilution of sample or standard is added to appropriate wells of a 96 well microtiter plate containing 10,000 cells/well. After forty-eight hours at 37°C and 5.5% CO₂, 0.5 μ Ci of methyl-³E-thymidine was added to each well. Eighteen hours later, the plates were then harvested and counted. A dose response curve (log rhG-CSF concentration vs. CPM-background) was generated and linear regression analysis of points which fall in the linear portion of the standard curve was performed. Concentrations of unknown test samples were determined using the resulting linear equation and correction for the dilution factor. Results: Results are presented in FIGURE 4. As can be seen, of the three monopegylated species, N-terminally monopegylated G-CSF demonstrates the highest in vitro biological activity.

5. In vivo activity. In vivo testing confirmed the activity of the N-terminally pegylated material. The in vivo testing was carried out by dosing male golden hamsters with a 0.1 mg/kg of sample, using a single subcutaneous injection. Four animals were subjected to terminal bleeds per group per time point. Serum samples were subject to a complete blood count on the same day that the samples were collected. The average white blood cell counts were calculated. As can be seen in FIGURES 5A and 5B, the response from each material peaks after one day following a single subcutaneous injection of 0.1 mg/kg. Two of the monopegylated materials, (N-terminal and Lys-35) showed prolonged responses, while the response for the protein pegylated at lysine 41 showed no increase in in vivo activity over unmodified rhG-CSF (indeed it shows less, FIGURE 5B). These results illustrate that attaching a single polyethylene glycol molecule can dramatically alter the therapeutic profile of a protein and that the benefit of pegylating a protein can be dependent upon the site of modification. The net average WBC area under the curve after the single subcutaneous injection (calculated according to CRC Standard Mathematical Tables, 26th Ed. (Beyer, W. H., Ed.) CRC Press Inc., Boca Raton, FL 1981. p. 125) was similar for the Lys-35 and N-terminal monopegylated material.

E. Stability Studies

[0065] In addition, stability studies were performed on the N-terminal and Lys-35 monopegylated material as prepared above. The Lys-41 material was not used as it demonstrated no additional activity beyond unmodified G-CSF. These studies demonstrate that the N-terminally pegylated G-CSF is unexpectedly more stable upon storage than the other form of monopegylated G-CSF, monopegylated lysine 35. Stability was assessed in terms of breakdown of product, as visualized using SEC-HPLC.

Methods: N-terminally pegylated G-CSF and lysine 35 monopegylated G-CSF were studied in two pH levels, pH 4.0 and pH 6.0 at 4°C, each for up to 16 days. Elevating the pH to 6.0 provides an environment for accelerated stability assays. For the pH 6.0 samples, N-terminal monopegylated G-CSF and lysine 35 monopegylated G-CSF as prepared above were placed in a buffer containing 20 mM sodium phosphate, 5 mM sodium acetate, 2.5 % mannitol, 0.005 % Tween-80, pH 6.0 at a final protein concentration of 0.25 mg/ml. One ml aliquots were stored in 3 ml sterile injection vials. Vials of each sample were stored at 4°C and 29°C for up to 16 days. Stability was assessed by SEC-HPLC tracings. If the later measurements stayed the same (as ascertained by visual inspection) as the initial (Time = 0) measurements, the sample was considered to be stable for that length of time.

Results:- Results are illustrated in FIGURES 6A-6C.

(a) Comparison at pH 6.0 at 4°C. FIGURE 6A shows the 4°C SEC-HPLC profiles for N-terminally monopegylated G-CSF at pH 6 over time and FIGURE 6B shows the 4°C SEC-HPLC profiles for lysine 35 monopegylated G-CSF at pH 6 over time. One interpretation is that the Lys-35 material is breaking down to a material with a molecular weight similar to that of unmodified G-CSF.

(b) Extended duration at pH 4.0 at 4°C. pH 4.0 and 4°C provides something of a control illustrating relatively stable conditions in that the N-terminal monopegylated material shows no degradation. For the Lys-35 monopegylated material, degradation of the material is still occurring, but at a much slower rate.

(c) Comparison at pH 6.0 at 4°C. FIGURES 6C illustrates the SEC-HPLC profiles for the monopegylated G-CSF's under these conditions, under extended time periods. As can be seen, at pH 6.0 and 4°C, the lysine 35 monopegylated material exhibits no increase in depegylation at day 16 or day 35 beyond what was seen for day 6 (FIGURE 6B). This indicates that depegylation. (instability) does not change, under those conditions, beyond day 6.

EXAMPLE 2

[0066] This example demonstrates a method of preparing a substantially homogenous population of monopegylated G-CSF using reductive alkylation, and characterization of this population. Recombinant G-CSF as described in example 1 was used. As can be seen, not only do the present methods provide advantages in terms of yield of N-terminally monopegylated material, but also, the amine linkages of the reductive alkylation process produce substantially more stable products as demonstrated by a large difference in the degree of aggregation upon storage.

A. Preparation of the mono-methoxypolyethylene glycol-G-CSF conjugates with the site of attachment at the N-terminal α -amino residue.

[0067] To a cooled (4°C), stirred solution of rhG-CSF (1 ml, 5 mg/ml as described in Example 1) in 100 mM sodium phosphate, pH 5, containing 20 mM NaCNBH₃, was added a 5-fold molar excess of methoxypolyethylene glycol aldehyde (MPEG) (average molecular weight, 6 kDa). The stirring of the reaction mixture was continued at the same temperature.

[0068] The extent of the protein modification during the course of the reaction was monitored by SEC-HPLC using Bio-Sil SEC 250-5 column (BIO-RAD) eluted with 0.05 M NaH₂PO₄, 0.05 M Na₂HPO₄, 0.15 M NaCl, 0.01 M NaN₃, pH 6.8 at 1 ml/min.

[0069] After 10 hours the SEC-HPLC analysis indicated that 92% of the protein has been converted to the mono-MPEG-G-CSF derivative. This can be seen in FIGURE 7, which is a recording of the protein concentration (as determined by absorbance at A280) and shows the peak eluting at 8.72 minutes as monopegylated G-CSF, and a minor peak of unreacted G-CSF eluting at 9.78 minutes.

[0070] As a comparison, FIGURE 8 shows the peaks obtained when using N-hydroxysuccinimide ester of MPEG. The molecular weight was also 6kDa. As can be seen, the mixture obtained from this reaction was: tri-MPEG-G-CSF conjugated (shoulder at approximately 7.25 minutes), di-MPEG-G-CSF conjugate (peak at 7.62 minutes), mono-MPEG-G-CSF conjugate (peak at 8.43 minutes) and unreacted G-CSF (peak at 9.87 minutes).

[0071] At this 10 hour time point, where 92% of the protein had been converted to monopegylated material, the pH of the reaction mixture was adjusted to pH 4 with 100 mM HCl and the reaction mixture was diluted 5 times with 1 mM HCl.

[0072] The mono-MPEG-G-CSF derivative was purified by ion exchange chromatography using HiLoad 16/10 S Sepharose HP column (Pharmacia) equilibrated with 20 mM sodium acetate buffer, pH 4. The reaction mixture was loaded on the column at a flow rate of 1 ml/min and the unreacted MPEG aldehyde eluted with three column volumes of the same buffer. Then a linear 400 minute gradient from 0% to 45% 20 mM sodium acetate, pH 4, containing 1 M NaCl was used to elute the protein-polymer conjugate at 4°C.

[0073] Fractions containing the mono-MPEG-G-CSF derivative were pooled, concentrated and sterile filtered.

[0074] Various mono-MPEG-G-CSF conjugates obtained by modifying rhG-CSF with MPEG aldehydes of different average molecular weight (12, 20 and 25 kDa) were prepared in a similar manner.

B. Analysis of Monopegylated G-CSF

1. Molecular Weight

[0075] The molecular weight of the monopegylated conjugates was determined by SDS-PAGE, gel filtration, matrix assisted laser desorption mass spectrometry, and equilibrium centrifugation. These results are presented in Table 4, below.

TABLE 4

Molecular Weights of N-terminally Alkylated Mono-MPEG-G-CSF Conjugates				
Conjugate	MW estimated	MW gel filtration	MW mass spectrometry	MW ultra-centrifugation
MPEG-(6kDa)-G-CSF	24800	53024	24737	25548
MPEG-(12kDa)-G-CSF	30800	124343	30703	29711
MPEG-(20kDa)-G-CSF	38800	221876	38577	38196
MPEG-(25kDa)-G-CSF	43800	333266	N/D	N/D

[0076] The structure of the prepared N-terminal mono-MPEG-G-CSF conjugates was confirmed using the methods

of N-terminal protein sequencing and peptide mapping. Cyanogen bromide cleavage of the N-terminal methionyl residue resulted in removal of the polyethylene glycol moiety.

2. Biological Activity

[0077] The *in vitro* biological activity of the monopegylated MPEG-G-CSF conjugates was determined by measuring the stimulated uptake of ^3H thymidine into mouse bone marrow cells.

[0078] The *in vivo* biological activity was determined by subcutaneous injection to hamsters mono-MPEG-G-CSF conjugates or rhG-CSF (at 100mg/kg) and measuring total white blood cell count. Bioactivity as compared to non-derivatized G-CSF was calculated as the area under the WBC/time curve after subtracting the vehicle control curve. Relative bioactivity of the mono-MPEG-G-CSF derivatives was expressed as the percentage bioactivity compared to unmodified G-CSF.

[0079] This is illustrated in FIGURE 9, which is a graph illustrating the total white blood cell response to mono-N-terminal MPEG-G-CSF conjugates prepared by reductive alkylation of rhG-CSF with MPEG aldehydes of different molecular weights (6 kDa, 12 kDa, and 20 kDa). As can be seen, all monopegylated molecules elicited a response. The higher the molecular weight of the polyethylene glycol moiety used, the higher the white blood cell count achieved, except the 12 kDa achieved a slightly higher count than did the 20 kDa version at day 2.

3. Stability Studies

[0080] N-terminally monopegylated G-CSF's prepared by the two different methods of Example 1 and 2 were compared for the degree of aggregation. Unexpectedly, N-terminally monopegylated G-CSF using the reductive alkylation method was found to be substantially more stable than N-terminally pegylated G-CSF with an amide linkage (NHS acylation as described in Example 1).

[0081] Methods: Both N-terminally pegylated G-CSF samples were in 10 mM NaOAc, pH 4.0 with 5% sorbitol, at a concentration of 1 mg protein/ml. The G-CSF's were pegylated with PEG 6000 for each. The amide-linked conjugate was prepared as in Example 1, and the amine linked conjugate was prepared as in Example 2. Six samples of each were stored for eight weeks at 45°C. At the end of eight weeks, the degree of aggregation was determined using size exclusion chromatography and ion exchange chromatography.

[0082] Results: The results demonstrate that the present reductive alkylation method is advantageous over the acylation method because, surprisingly, it produces a material with far fewer aggregates after 8 weeks at elevated temperatures. The table below shows the percent of non-aggregated material ("main peak" material) for both materials using size exclusion chromatography (SEC) or ion exchange (IE):

TABLE 5

Sample: 8 wks, 45°C	% Main Peak SEC/IE
Amine	82%/84%
Amide	37%/65%*

* This is relatively high because ion exchange does not allow for full analysis of the aggregation.

SEQUENCE LISTING

[0083]

(1) GENERAL INFORMATION:

(i) APPLICANT: AMGEN INC.

(ii) TITLE OF INVENTION: N-Terminally monopegylated G-CSF or an analog thereof.

(iii) NUMBER OF SEQUENCES: 2

(iv) CORRESPONDENCE ADDRESS:

(A) ADDRESSEE: Amgen Inc.

(B) STREET: 1840 Dehavilland Drive

(C) CITY: Thousand Oaks
 (D) STATE: California
 (E) COUNTRY: USA
 (F) ZIP: 91320

(v) COMPUTER READABLE FORM:

(A) MEDIUM TYPE: Floppy disk
 (B) COMPUTER: IBM PC compatible
 (C) OPERATING SYSTEM: PC-DOS/MS-DOS
 (D) SOFTWARE: PatentIn Release #1.0, Version #1.25

(vi) CURRENT APPLICATION DATA:

(A) APPLICATION NUMBER:
 (B) FILING DATE:
 (C) CLASSIFICATION:

(viii) ATTORNEY/AGENT INFORMATION:

(A) NAME: Pessin, Karol M.
 (C) REFERENCE/DOCKET NUMBER: A-286

(2) INFORMATION FOR SEQ ID NO:1:

(i) SEQUENCE CHARACTERISTICS:

(A) LENGTH: 531 base pairs
 (B) TYPE: nucleic acid
 (C) STRANDEDNESS: single
 (D) TOPOLOGY: linear

(ii) MOLECULE TYPE: cDNA

(xi) SEQUENCE DESCRIPTION: SEQ ID NO:1:

ATGACTCCAT TAGGTCCTGC TTCTTCTCTG CCGCAAAGCT TTCTGCTGAA ATGTCTGGAA	60
CAGGTTTCGTA AAATCCAGGG TGACGGTGCT GCACTGCAAG AAAAACTGTG CGCTACTTAC	120
AAACTGTGCC ATCCGGAAGA GCTGGTACTG CTGGGTCATT CTCTTGGGAT CCCGTGGGCT	180
CCGCTGTCTT CTGTGCCATC TCAAGCTCTT CAGCTGGCTG GTTGTCTGTC TCAACTGCAT	240
TCTGGTCTGT TCCTGTATCA GGGTCTTCTG CAAGCTCTGG AAGGTATCTC TCCGGAAGTG	300
GGTCCGACTC TGGACACTCT GCAGCTAGAT GTAGCTGACT TTGCTACTAC TATTTGGCAA	360
CAGATGGAAG AGCTCGGTAT GGCACCAGCT CTGCAACCGA CTCAAGGTGC TATGCCGGCA	420
TTCGCTTCTG CATTCCAGCG TCGTGCAGGA GGTGTACTGG TTGCTTCTCA TCTGCAATCT	480
TTCTTGAAG TATCTTACCG TGTTCTGCGT CATCTGGCTC AGCCGTAATA G	531

(2) INFORMATION FOR SEQ ID NO:2:

(i) SEQUENCE CHARACTERISTICS:

(A) LENGTH: 175 amino acids

(B) TYPE: amino acid

(C) STRANDEDNESS: single

(D) TOPOLOGY: linear

(ii) MOLECULE TYPE: G-CSF

(xi) SEQUENCE DESCRIPTION: SEQ ID NO:2:

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Met Thr Pro Leu Gly Pro Ala Ser Ser Leu Pro Gln Ser Phe Leu Leu
1           5           10           15

Lys Cys Leu Glu Gln Val Arg Lys Ile Gln Gly Asp Gly Ala Ala Leu
          20           25           30

Gln Glu Lys Leu Cys Ala Thr Tyr Lys Leu Cys His Pro Glu Glu Leu
          35           40           45

Val Leu Leu Gly His Ser Leu Gly Ile Pro Trp Ala Pro Leu Ser Ser
          50           55           60

Cys Pro Ser Gln Ala Leu Gln Leu Ala Gly Cys Leu Ser Gln Leu His
65           70           75           80

Ser Gly Leu Phe Leu Tyr Gln Gly Leu Leu Gln Ala Leu Glu Gly Ile
          85           90           95

Ser Pro Glu Leu Gly Pro Thr Leu Asp Thr Leu Gln Leu Asp Val Ala
          100          105          110

Asp Phe Ala Thr Thr Ile Trp Gln Gln Met Glu Glu Leu Gly Met Ala
          115          120          125

Pro Ala Leu Gln Pro Thr Gln Gly Ala Met Pro Ala Phe Ala Ser Ala
          130          135          140

Phe Gln Arg Arg Ala Gly Gly Val Leu Val Ala Ser His Leu Gln Ser
145          150          155          160

Phe Leu Glu Val Ser Tyr Arg Val Leu Arg His Leu Ala Gln Pro
          165          170          175

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Claims

1. A substantially homogenous preparation of N-terminally monopegylated G-CSF or an analog thereof, optionally in a pharmaceutically acceptable diluent, carrier or adjuvant.
2. A preparation of claim 1, where said polyethylene glycol has a molecular weight of between about 2 kDa and 100

kDa.

3. A preparation of claim 2 wherein said polyethylene glycol has a molecular weight of between about 6 kDa and 25 kDa.
4. A preparation of any one of claims 1 to 3 wherein said preparation is comprised of at least 90% N-terminally monopegylated G-CSF or analog thereof and at most 10% unpegylated G-CSF or analog thereof.
5. A preparation of claim 4 wherein said preparation is comprised of at least 95% N-terminally monopegylated G-CSF or analog thereof and at most 5% unpegylated G-CSF or analog thereof.
6. A preparation of any one of claims 1 to 5 wherein said G-CSF has the sequence identified in SEQ. ID No. 1.
7. A substantially homogenous preparation of N-terminally monopegylated G-CSF, wherein: (a) said G-CSF has the amino acid sequence identified in SEQ. ID No. 1; (b) said G-CSF is monopegylated with a polyethylene glycol moiety having a molecular weight of about 12 kDa.
8. A mixed preparation of G-CSF or analog thereof comprising a preparation of N-terminally monopegylated G-CSF or analog thereof mixed with a preparation of multipegylated G-CSF or analog thereof wherein the proportion of said preparation of monopegylated G-CSF or analog thereof is predetermined.
9. A mixed preparation of claim 8 wherein said preparation of N-terminally monopegylated G-CSF is selected from among those of claims 1 to 7.
10. A pharmaceutical composition comprising an effective amount of a preparation selected from among those according to any one of claims 1 to 9, in a pharmaceutically acceptable diluent, adjuvant or carrier.
11. Use of a preparation according to any one of claims 1 to 9 for the manufacture of a medicament for the treatment of a disorder characterized by a reduced hematopoietic or immune function.
12. A use according to claim 11 wherein said disorder is a result of chemotherapy, radiation therapy, infectious disease, severe chronic neutropenia, or leukemia.
13. A process for preparing N-terminally monopegylated G-CSF or an analog thereof comprising the steps of
 - a) reacting in an aqueous medium G-CSF or its analog having an alpha-amino-group at its N-terminus with a water-soluble polyethylene glycol having a single aldehyde group under conditions of a reductive alkylation and at a pH sufficiently acidic to selectively activate the alpha amino-group and
 - b) optionally separating the N-terminally monopegylated product from the reaction mixture.
14. A process according to claim 13 wherein the polyethylene glycol used has a molecular weight of between about 2 kDa and 100 kDa.
15. A process according to claim 14, wherein the polyethylene glycol used has a molecular weight of between about 6 kDa and 25 kDa.
16. A process according to any one of claims 13 to 15, wherein the polyethylene glycol used is a methoxy polyethylene glycol aldehyde.
17. A process according to any one of claims 13 to 16 wherein the reducing agent used in the reductive alkylation is sodium borohydride or sodium cyano borohydride.
18. A process according to any one of claims 13 to 17 wherein the G-CSF or its analog used is non-glycosylated.
19. A process according to any one of claims 13 to 18 wherein the G-CSF or its analog used has a methionine moiety at its N-terminus at position -1.

20. A process according to any one of claims 13 to 19 wherein the separation step (b) comprises a purification.
21. A process according to claim 20, wherein the purification comprises ion exchange chromatography of the reaction mixture and size exclusion chromatography.

Patentansprüche

1. Eine im wesentlichen homogene Zubereitung von N-terminal monopegyliertem G-CSF oder einem Analogon hiervon, gegebenenfalls mit einem pharmazeutisch verträglichen Verdünnungsmittel, Träger oder Hilfsstoff.
2. Eine Zubereitung gemäß Anspruch 1, wobei das Polyethylenglykol ein Molekulargewicht zwischen etwa 2 kDa und 100 kDa hat.
3. Eine Zubereitung gemäß Anspruch 2, wobei das Polyethylenglykol ein Molekulargewicht zwischen etwa 6 kDa und 25 kDa hat.
4. Eine Zubereitung gemäß einem der Ansprüche 1 bis 3, wobei die Zubereitung umfaßt mindestens 90% N-terminal monopegyliertes G-CSF oder ein Analogon hiervon und höchstens 10% unpegyliertes G-CSF oder ein Analogon hiervon.
5. Eine Zubereitung gemäß Anspruch 4, wobei die Zubereitung umfaßt mindestens 95% N-terminal monopegyliertes G-CSF oder ein Analogon hiervon und höchstens 5% unpegyliertes G-CSF oder ein Analogon hiervon.
6. Eine Zubereitung gemäß einem der Ansprüche 1 bis 5, wobei das G-CSF die Sequenz gemäß SEQ ID NO:1 hat.
7. Eine im wesentlichen homogene Zubereitung von N-terminal monopegyliertem G-CSF, wobei
 - (a) das G-CSF die Aminosäuresequenz gemäß SEQ ID NO:1 hat;
 - (b) das G-CSF monopegyliert ist mit einem Polyethylenglykolrest mit einem Molekulargewicht von etwa 12 kDa.
8. Eine gemischte Zubereitung von G-CSF oder einem Analogon hiervon, umfassend eine Zubereitung eines N-terminal monopegylierten G-CSF oder einem Analogon hiervon, gemischt mit einer Zubereitung von multipegyliertem G-CSF oder einem Analogon hiervon, wobei der Teil der Zubereitung des monopegylierten G-CSF oder des Analogons hiervon festgelegt ist.
9. Eine gemischte Zubereitung gemäß Anspruch 8, wobei die Zubereitung des N-terminal monopegylierten G-CSF ausgewählt ist unter denen der Ansprüche 1 bis 7.
10. Eine pharmazeutische Zusammensetzung, umfassend eine wirksame Menge einer Zubereitung ausgewählt unter denen gemäß einem der Ansprüche 1 bis 9 in einem pharmazeutisch verträglichen Verdünnungsmittel, Hilfsmittel oder Trägerstoff.
11. Verwendung einer Zubereitung gemäß einem der Ansprüche 1 bis 9 zur Herstellung eines Medikaments zur Behandlung einer Störung, charakterisiert durch eine reduzierte Hämatopoese oder Immundefizienz.
12. Verwendung gemäß Anspruch 11, wobei die Störung das Ergebnis einer Chemotherapie, Bestrahlungstherapie, Infektionskrankheit, schweren chronischen Neutropenie oder Leukämie ist.
13. Ein Verfahren zur Herstellung von N-terminal monopegyliertem G-CSF oder einem Analogon hiervon, umfassend die Schritte:
 - a) das Umsetzen in einem wäßrigen Medium von G-CSF oder seinem Analogon mit einer alpha-Aminogruppe an seinem N-terminalen Ende mit einem wasserlöslichen Polyethylenglykol mit einer einzelnen Aldehydgruppe unter Bedingungen einer reduktiven Alkylierung und bei einem pH-Wert ausreichend sauer, um selektiv die alpha-Aminogruppe zu aktivieren und gegebenenfalls

b) Trennung des N-terminalen monopegylierten Produkts von dem Reaktionsgemisch.

14. Ein Verfahren gemäß Anspruch 13, wobei das verwendete Polyethylenglykol ein Molekulargewicht zwischen etwa 2 kDa und 100 kDa hat.
15. Ein Verfahren gemäß Anspruch 14, wobei das verwendete Polyethylenglykol ein Molekulargewicht zwischen etwa 6 kDa und 25 kDa hat.
16. Ein Verfahren gemäß einem der Ansprüche 13 bis 15, wobei das verwendete Polyethylenglykol ein Methoxypolyethylenglykolaldehyd ist.
17. Ein Verfahren gemäß einem der Ansprüche 13 bis 16, wobei das verwendete reduzierende Mittel in der reduktiven Alkylierung Natriumborhydrid oder Natriumcyanoborhydrid ist.
18. Ein Verfahren gemäß einem der Ansprüche 13 bis 17, wobei das verwendete G-CSF oder sein Analogon nicht glykosyliert ist.
19. Ein Verfahren gemäß einem der Ansprüche 13 bis 18, wobei das verwendete G-CSF oder sein Analogon einen Methioninrest an dem N-Terminus an Position -1 hat.
20. Ein Verfahren gemäß einem der Ansprüche 13 bis 19, wobei der Trennungsschritt (b) die Reinigung umfaßt.
21. Ein Verfahren gemäß Anspruch 20, wobei der Reinigungsschritt die Ionenaustauscherchromatographie des Reaktionsgemisches und die Größenausschlußchromatographie umfaßt.

Revendications

1. Préparation en grande partie homogène de G-CSF à terminaisons N monopéglées ou d'un analogue de celui-ci, éventuellement dans un diluant, support ou adjuvant pharmaceutiquement acceptable.
2. Préparation selon la revendication 1, où ledit polyéthylèneglycol a un poids moléculaire d'environ 2 kDa à 100 kDa.
3. Préparation selon la revendication 2 dans laquelle ledit polyéthylèneglycol a un poids moléculaire d'environ 6 kDa à 25 kDa.
4. Préparation selon l'une quelconque des revendications 1 à 3 dans laquelle ladite préparation est constituée à 90% au moins de G-CSF à terminaisons N monopéglées ou d'un analogue de celui-ci et à 10% au plus de G-CSF non péglé ou d'un analogue de celui-ci.
5. Préparation selon la revendication 4 dans laquelle ladite préparation est constituée à 95% au moins de G-CSF à terminaisons N monopéglées ou d'un analogue de celui-ci et à 5% au plus de G-CSF non péglé ou d'un analogue de celui-ci.
6. Préparation selon l'une quelconque des revendications 1 à 5 dans laquelle ledit G-CSF possède la séquence identifiée dans SEQ. ID No. 1.
7. Préparation en grande partie homogène de G-CSF à terminaisons N monopéglées, dans laquelle : (a) ledit G-CSF possède la séquence d'acides aminés identifiée dans SEQ. ID No. 1; (b) ledit G-CSF est monopéglé avec un fragment polyéthylèneglycol ayant un poids moléculaire d'environ 12 kDa.
8. Préparation mixte de G-CSF ou d'un analogue de celui-ci, comprenant une préparation de G-CSF à terminaisons N monopéglées ou d'un analogue de celui-ci mélangée avec une préparation de G-CSF multipéglé ou d'un analogue de celui-ci, dans laquelle la proportion de ladite préparation de G-CSF monopéglé ou d'un analogue de celui-ci est prédéterminée.
9. Préparation mixte selon la revendication 8 dans laquelle ladite préparation de G-CSF à terminaisons N monopéglées est choisie parmi celles des revendications 1 à 7.

10. Composition pharmaceutique comprenant une quantité efficace d'une préparation choisie parmi celles selon l'une quelconque des revendications 1 à 9, dans un diluant, adjuvant ou support pharmaceutiquement acceptable.
- 5 11. Utilisation d'une préparation selon l'une quelconque des revendications 1 à 9 pour la préparation d'un médicament destiné au traitement d'un dérèglement caractérisé par une fonction hématopoïétique ou immunitaire amoindrie.
12. Utilisation selon la revendication 11 où ledit dérèglement est le résultat d'une chimiothérapie, d'une radiothérapie, d'une maladie infectieuse, d'une neutropénie chronique grave, ou d'une leucémie.
- 10 13. Procédé de préparation de G-CSF à terminaisons N monopétylées ou d'un analogue de celui-ci, comportant les étapes consistant à
 - 15 a) faire réagir dans un milieu aqueux du G-CSF ou son analogue ayant un groupe alpha-amino à son extrémité N-terminale avec un polyéthylèneglycol hydrosoluble ayant un seul groupe aldéhyde dans des conditions d'alkylation réductrice et à un pH suffisamment acide pour activer sélectivement le groupe alpha-amino et, éventuellement,
 - b) séparer le produit à terminaisons N monopétylées du mélange réactionnel.
- 20 14. Procédé selon la revendication 13 dans lequel le polyéthylèneglycol utilisé a un poids moléculaire d'environ 2 kDa à 100 kDa.
- 15 15. Procédé selon la revendication 14 dans lequel le polyéthylèneglycol utilisé a un poids moléculaire d'environ 6 kDa à 25 kDa.
- 25 16. Procédé selon l'une quelconque des revendications 13 à 15 dans lequel le polyéthylèneglycol utilisé est un méthoxypolyéthylèneglycol aldéhyde.
17. Procédé selon l'une quelconque des revendications 13 à 16 dans lequel l'agent réducteur utilisé dans l'alkylation réductrice est le borohydrure de sodium ou le cyanoborohydrure de sodium.
- 30 18. Procédé selon l'une quelconque des revendications 13 à 17 dans lequel le G-CSF ou son analogue utilisé est non glycosylé.
- 35 19. Procédé selon l'une quelconque des revendications 13 à 18 dans lequel le G-CSF ou son analogue utilisé a un résidu de méthionine à son extrémité N-terminale en position -1.
20. Procédé selon l'une quelconque des revendications 13 à 19 dans lequel l'étape de séparation (b) comprend une purification.
- 40 21. Procédé selon la revendication 20 dans lequel la purification comprend une chromatographie d'échange d'ions du mélange réactionnel et une chromatographie d'exclusion.

Fig. 1A

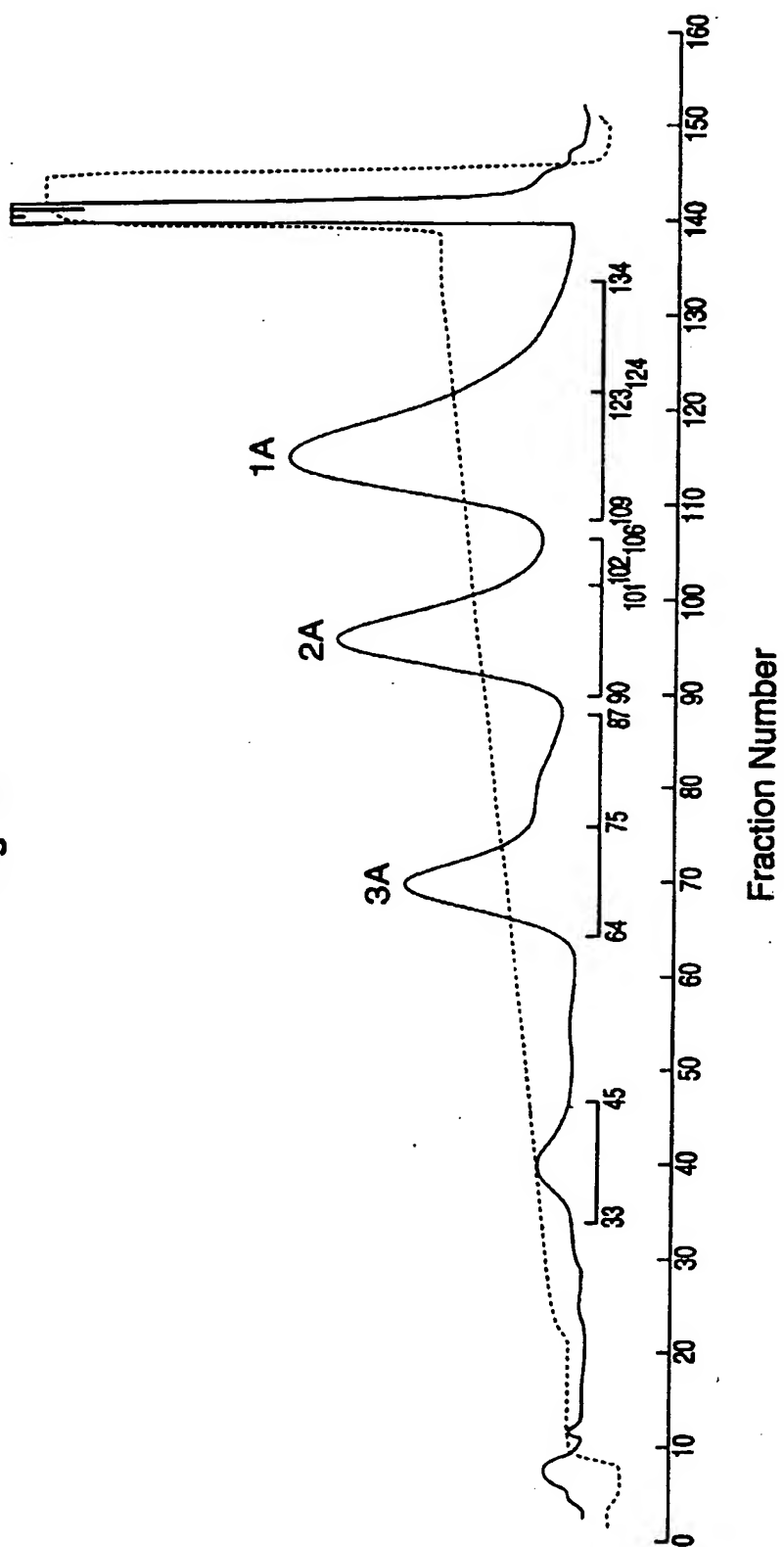
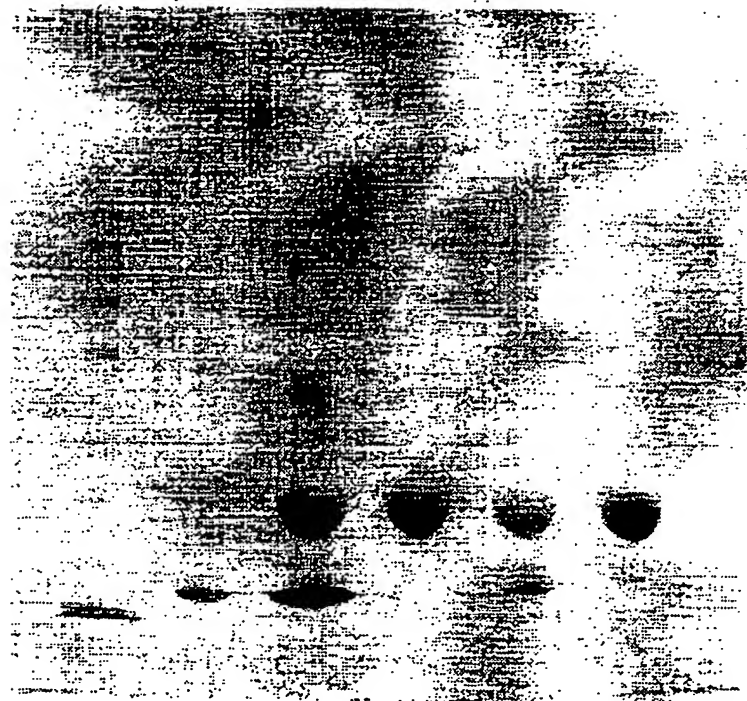


Fig. 1B

Lane No. 1 2 3 4 5 6

Lane No.	Sample	ug loaded
1	MW Protein Standards	-
2	rHuG-CSF Std	3.0
3	SCM-PEG-GCSF Reaction Mix	10.0
4	Species 1 (N-Term)	10.0
5	Species 2 (Lys-35)	10.0
6	Species 3 (Lys-41)	10.0

Fig. 2

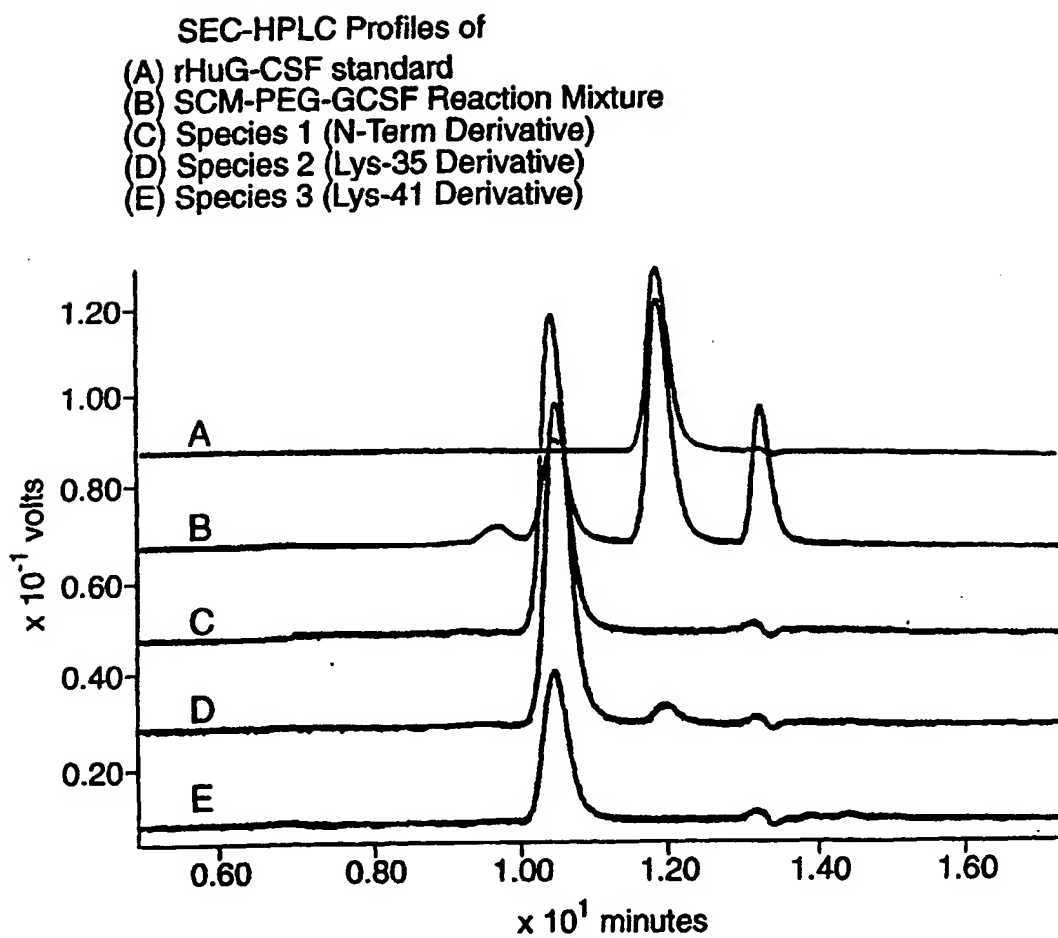


Fig. 3A

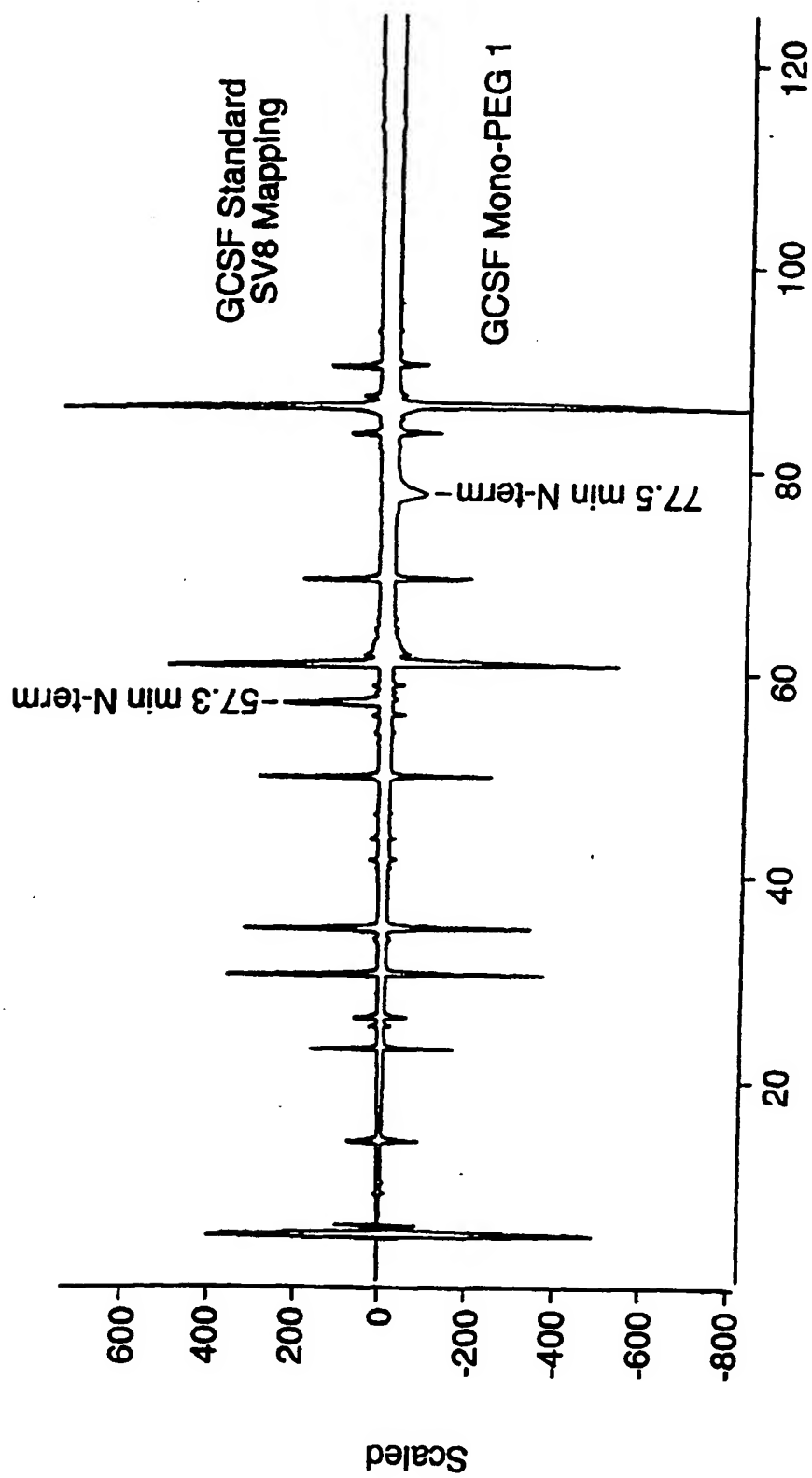


Fig. 3B

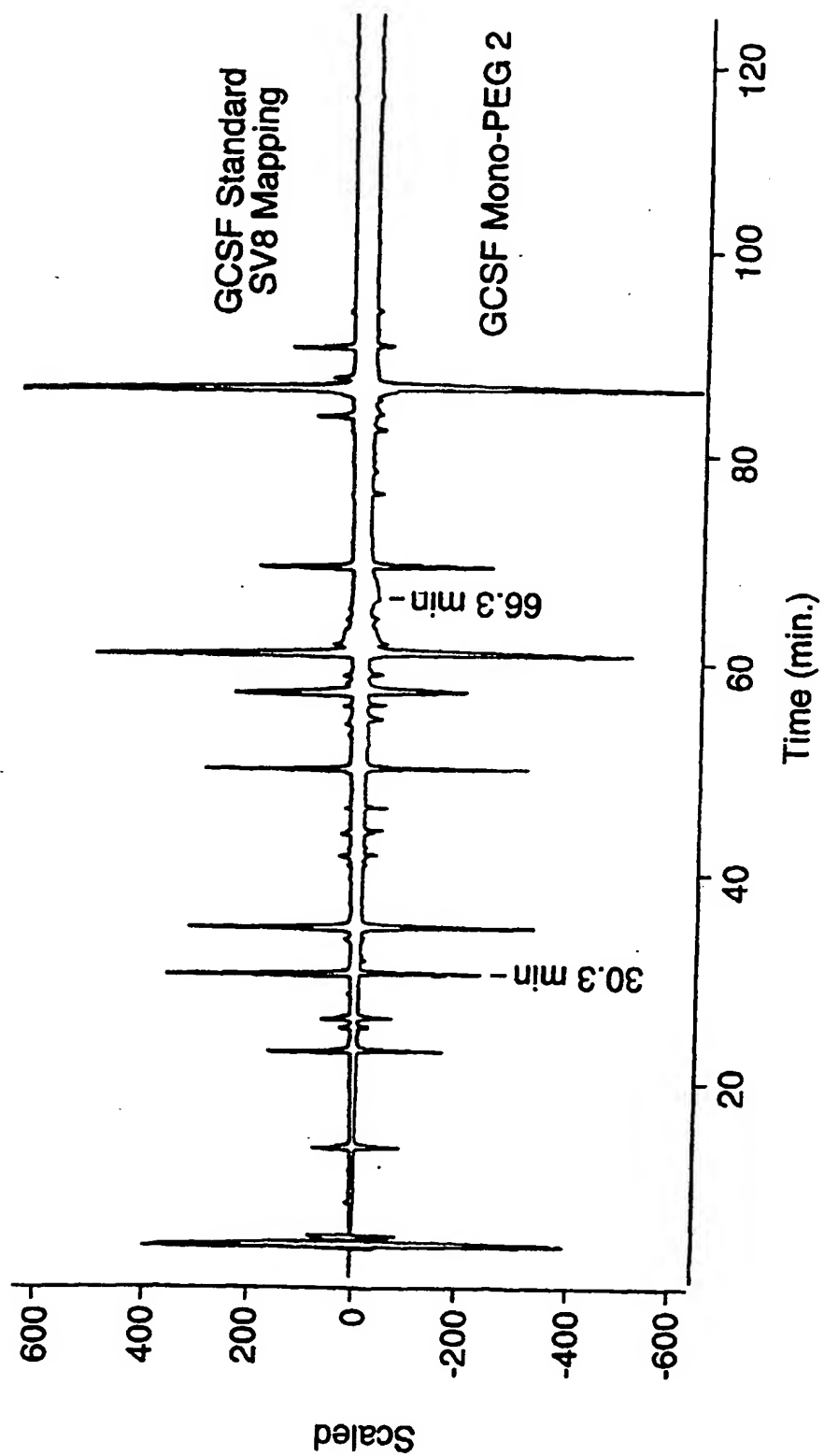


Fig. 3C

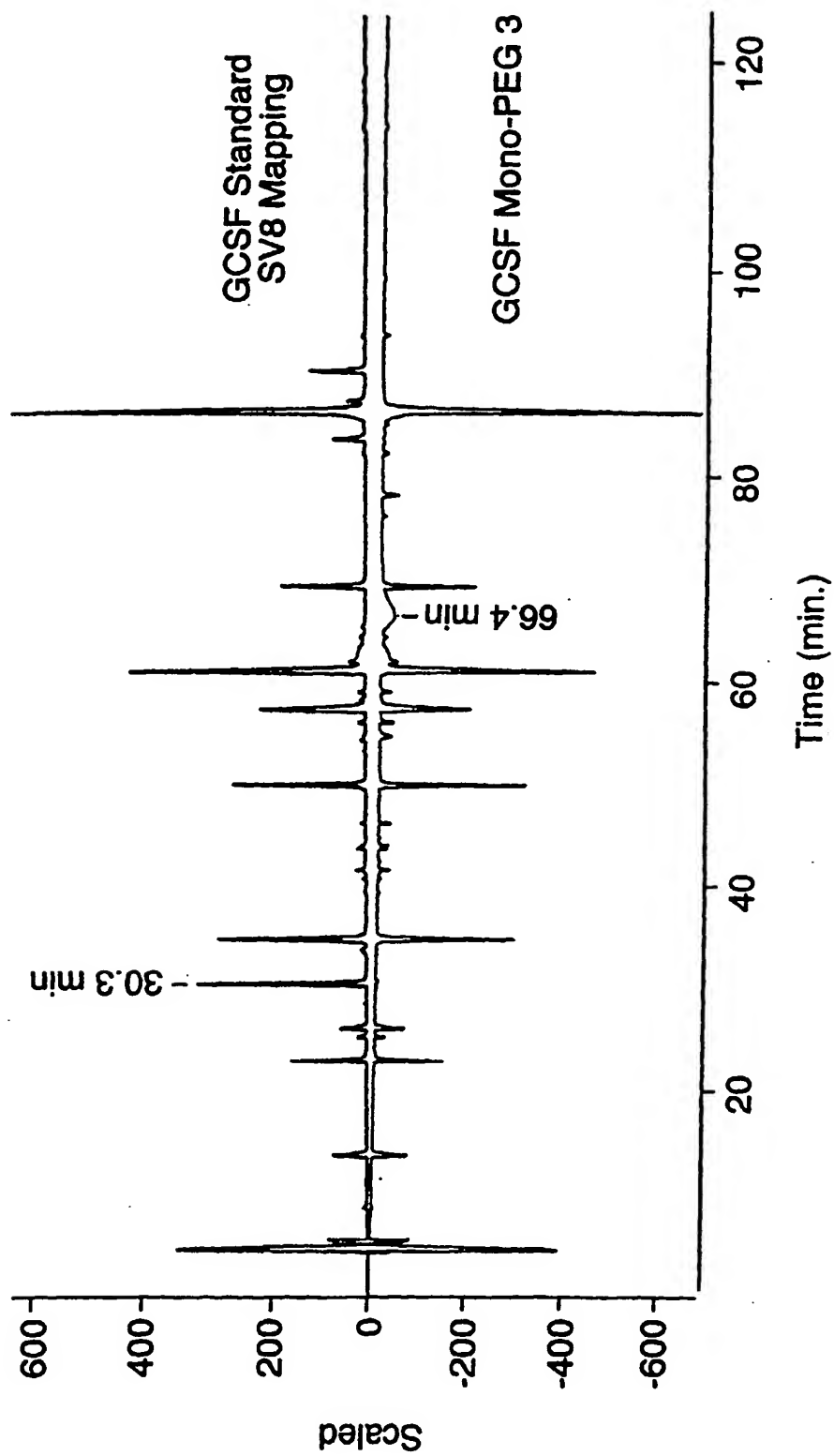
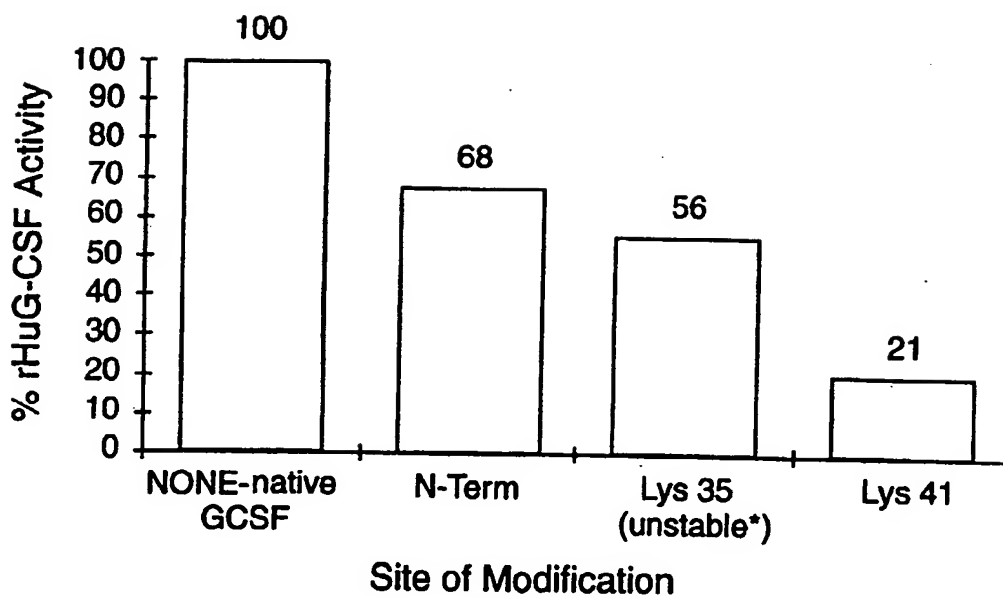


Fig. 4



* contains de-Pegylated rHuG-CSF, generated during storage.

Fig. 5A

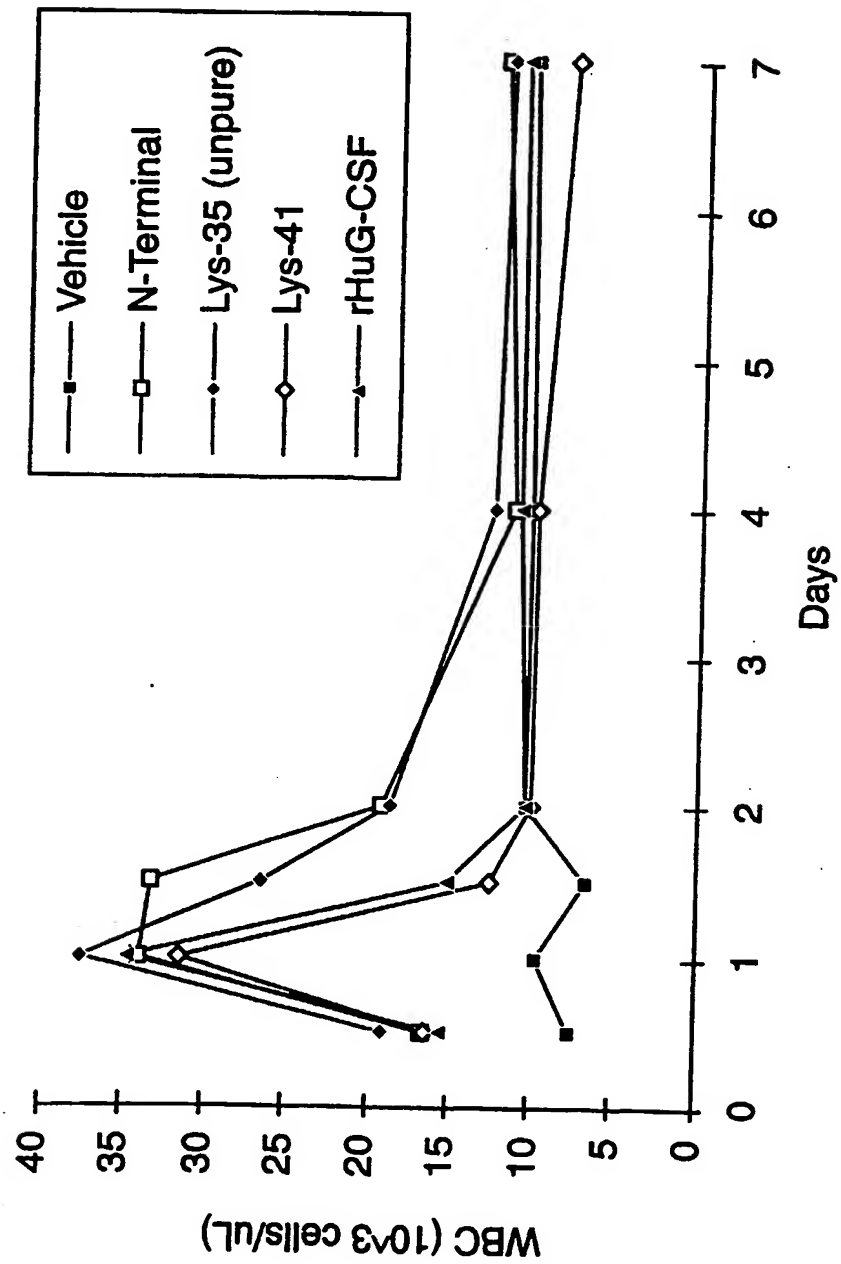


Fig. 5B

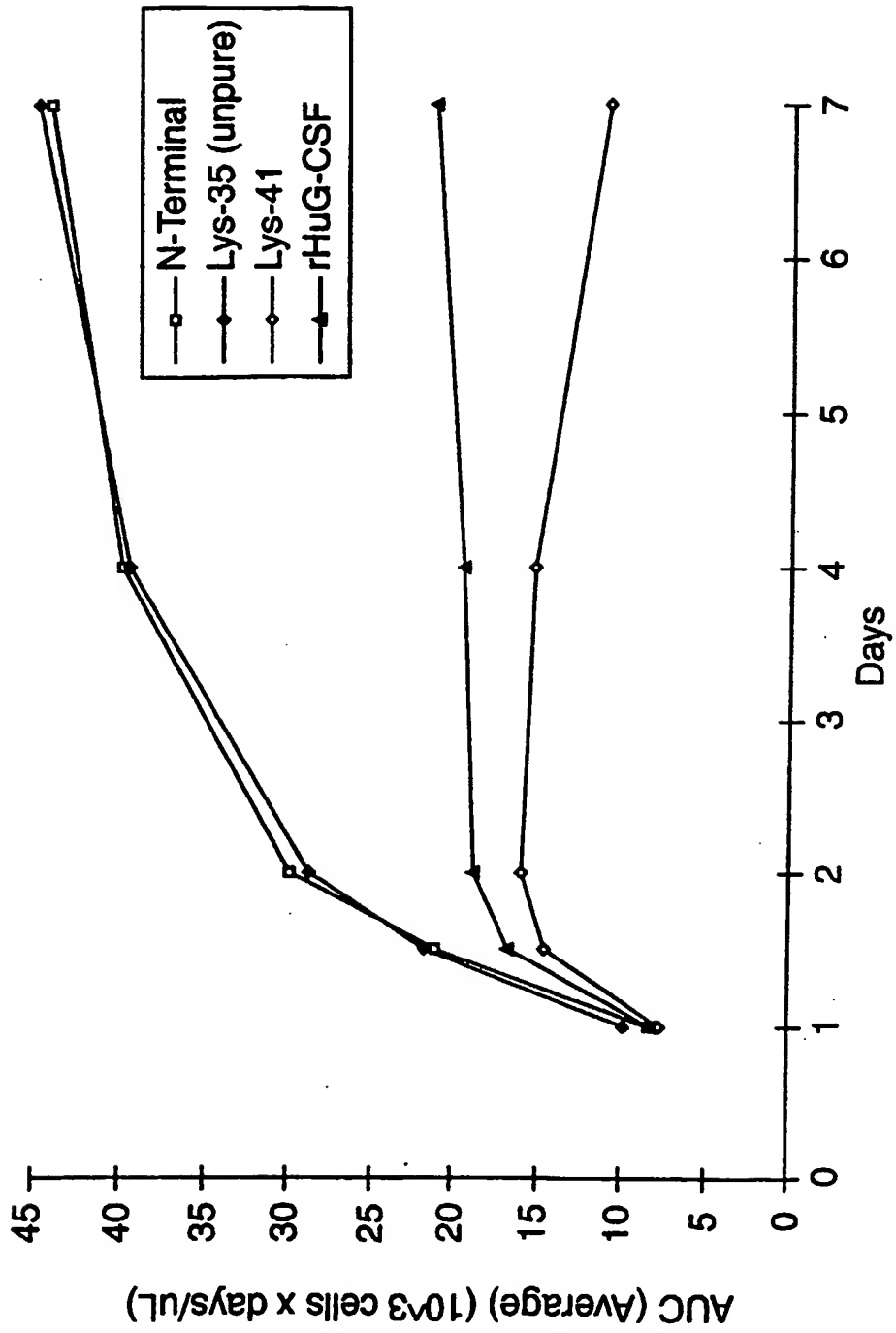


Fig. 6A

N-term monopegylated G-CSF, pH 6

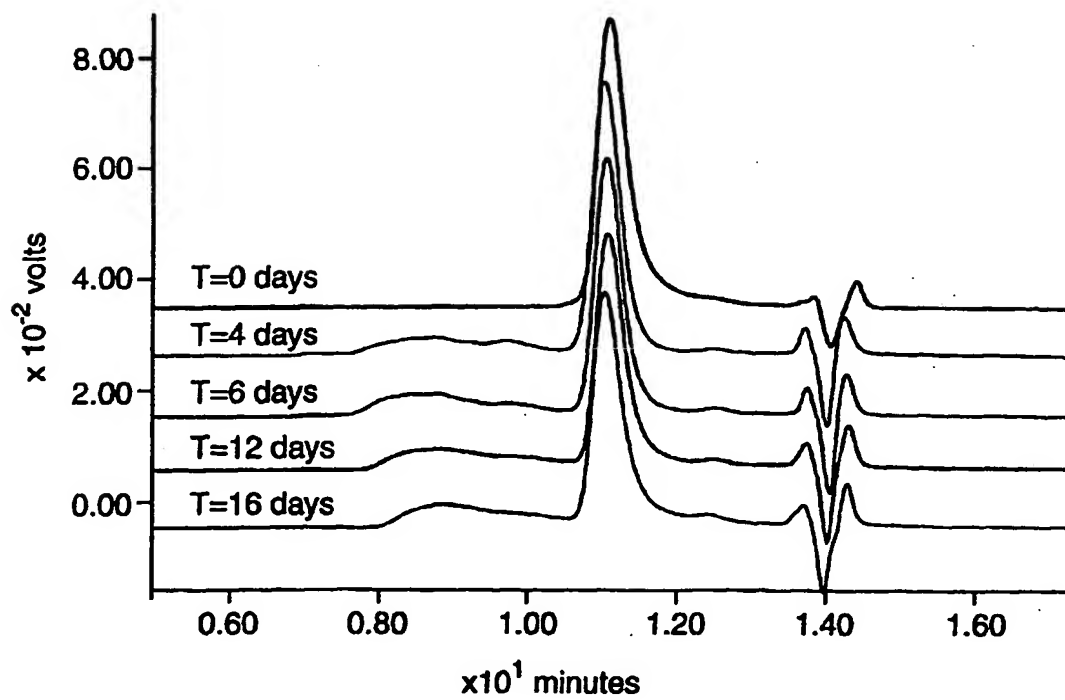


Fig. 6B

Lys 35 monopegylated G-CSF, pH 6

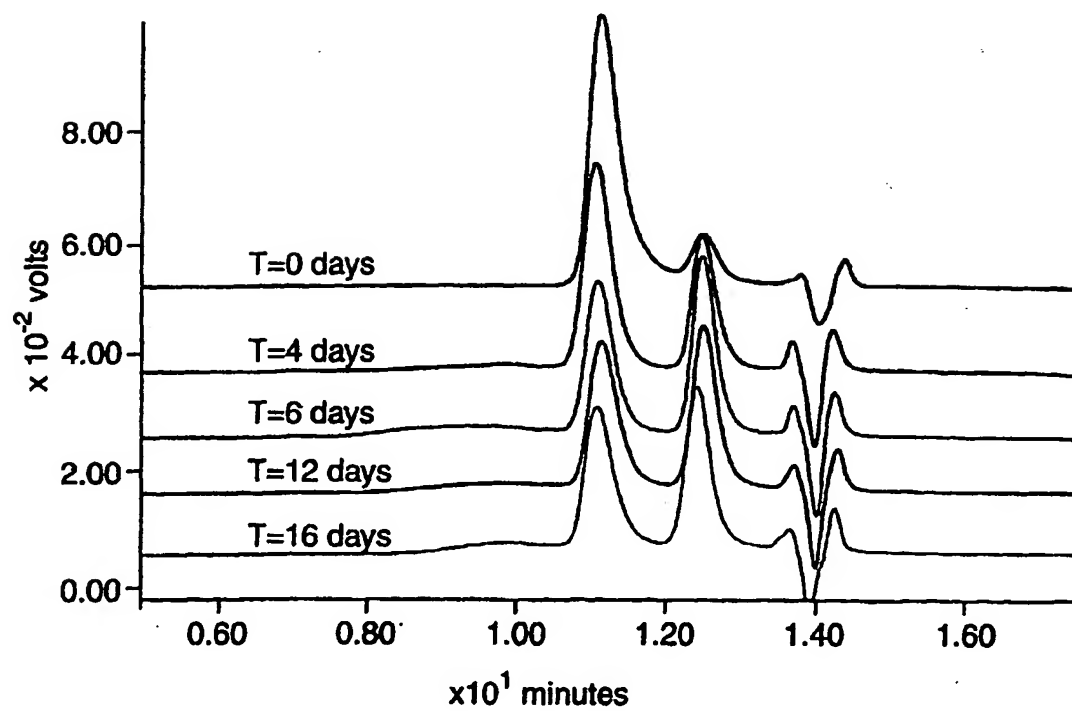


Fig. 6C

Lys 35 monopegylated G-CSF, pH 7

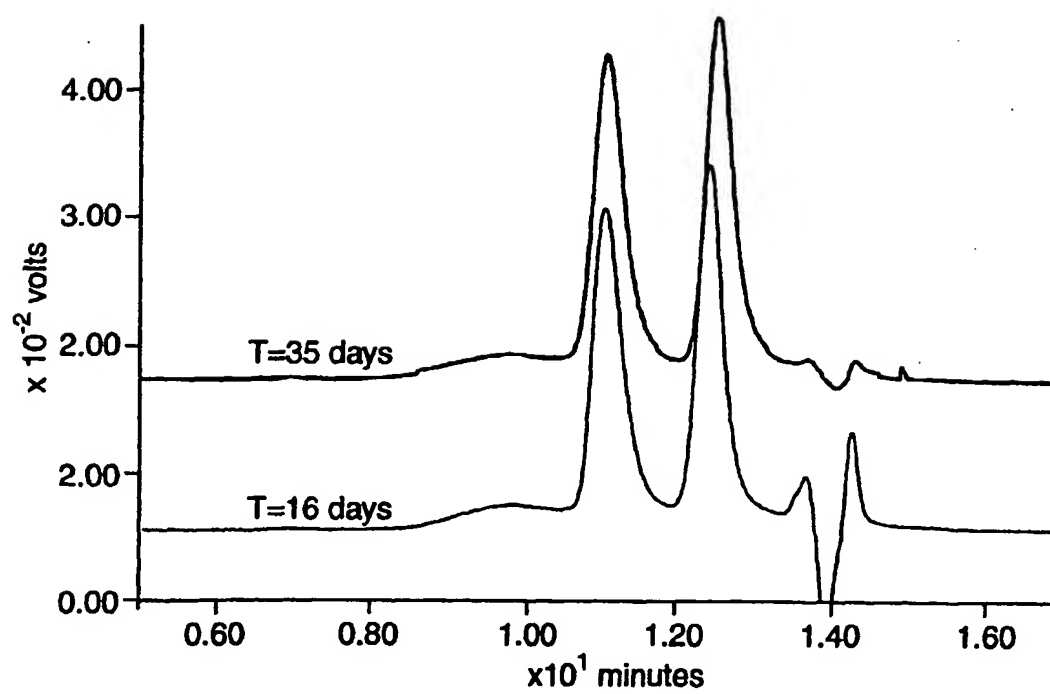


Fig. 7

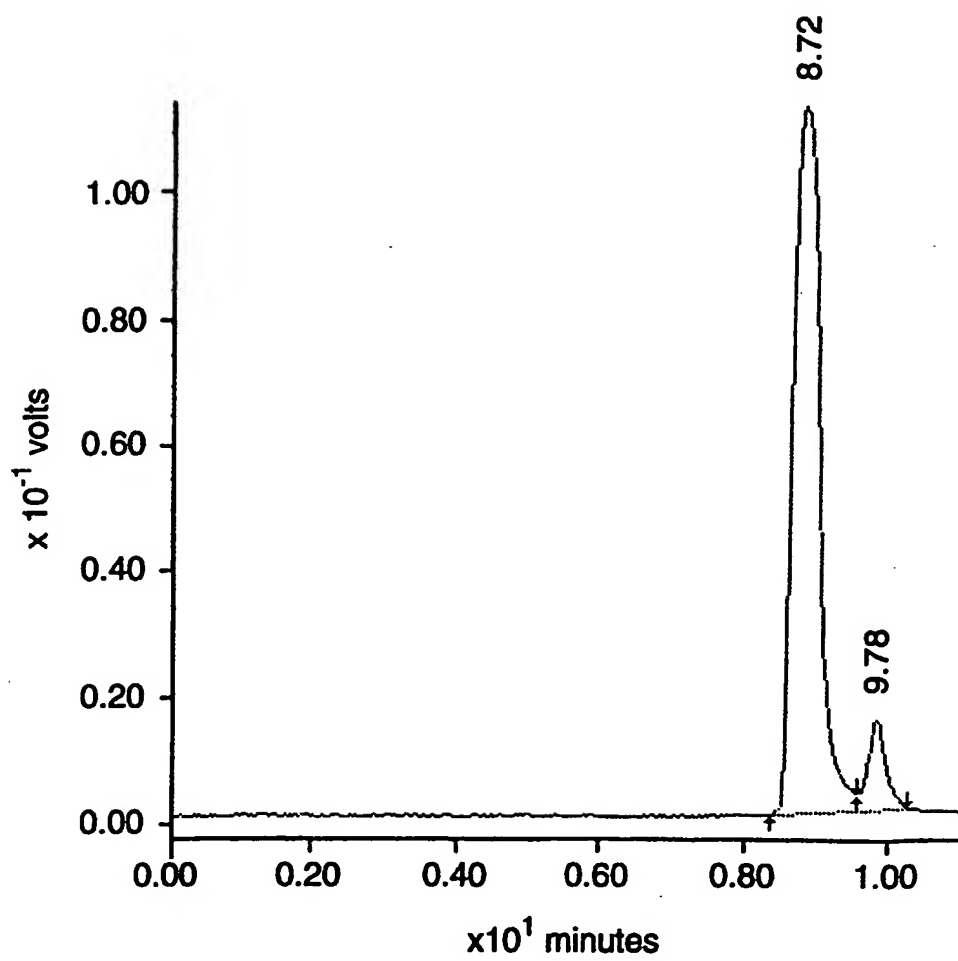


Fig. 8

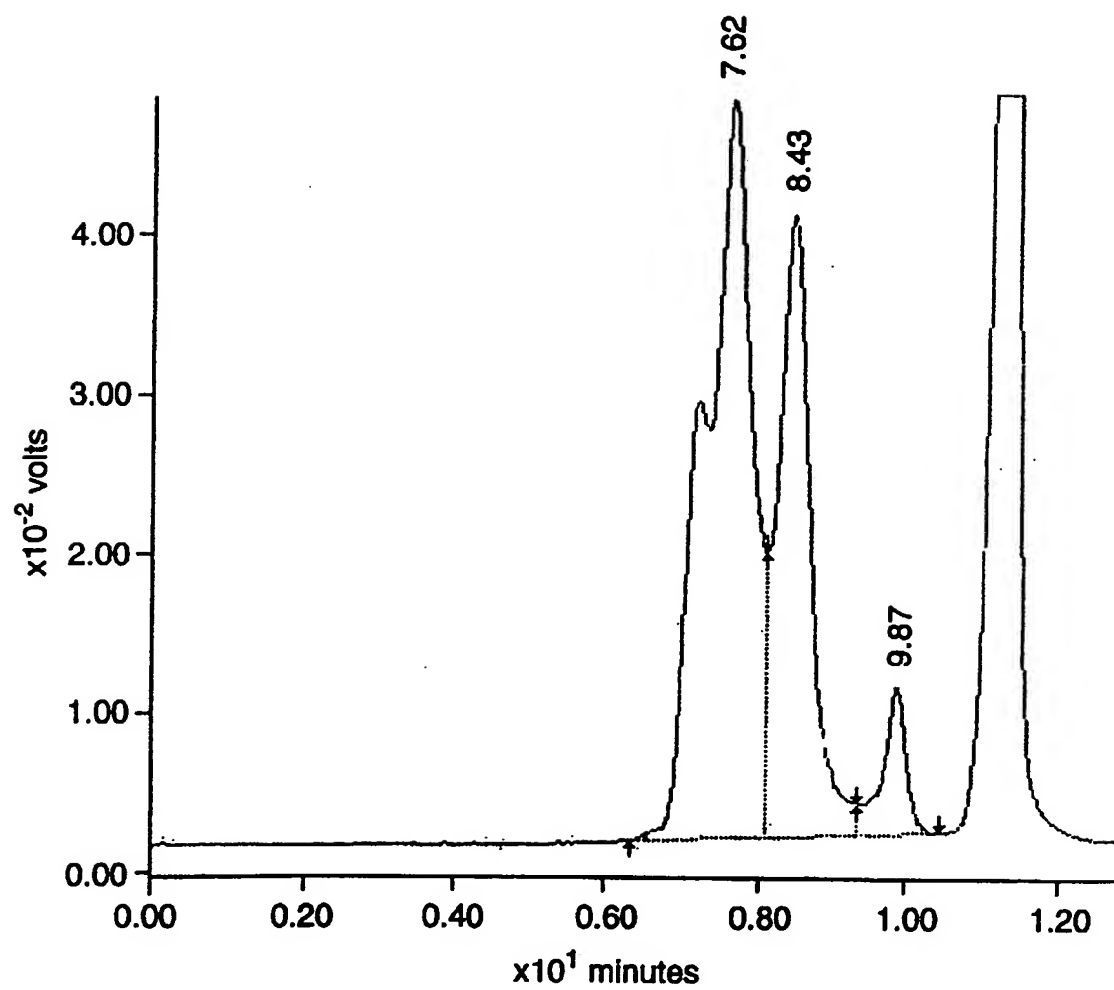


Fig. 9

